

DalSy: diffuser-aided sub-THz imaging system

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Abstract: Sub-terahertz (Sub-THz) waves possess exceptional attributes, capable of penetrating non-metallic and non-polarized materials while ensuring bio-safety. However, their practicality in imaging is marred by the emergence of troublesome speckle artifacts, primarily due to diffraction effects caused by wavelengths comparable to object dimensions. In addressing this limitation, we present the Diffuser-aided sub-THz Imaging System (DaISy), which utilizes a diffuser and a focusing lens to convert coherent waves into incoherent counterparts. The cornerstone of our progress lies in a coherence theory-based theoretical framework, pivotal for designing and validating the THz diffuser, and systematically evaluating speckle phenomena. Our experimental results utilizing DaISy reveal substantial improvements in imaging quality and nearly diffraction-limited spatial resolution. Moreover, we demonstrate a tangible application of DaISy in the scenario of security scanning, highlighting the versatile potential of sub-THz waves in miscellaneous fields.

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1. Introduction

Terahertz (THz) region (100 GHz to 10 THz) of the electromagnetic spectrum has experienced remarkable development and found diverse applications across various fields. Applications of THz technology range from high data-rate communication systems [1] to molecular spectroscopy [2], remote sensing [3], collision-availability studies [4], and non-destructive imaging [5,6]. Significantly, THz waves demonstrate exceptional transmission properties through non-metallic and non-polar mediums [7], rendering them highly suitable for a wide array of applications. Furthermore, the bio-safety profile of THz radiation, attributed to its low quantum photon energy in the meV range, further improves its suitability for practical applications [8-10]. As a result, THz imaging has become prominent in fields like biometrics, industry, and security, including the detection of illicit drugs [11] and non-destructive identification of electronic circuits [12]. Nonetheless, the practical viability of THz imaging systems faces limitations due to the low-power nature of their THz sources and the high absorption characteristics in polarized materials. These factors hinder their effectiveness in various imaging applications. Within the broader THz region, the sub-THz range (100-300 GHz) is particularly advantageous for certain applications, utilizing high-power illumination and relatively lower absorption coefficients in polarized materials to achieve improved depth in imaging [13,14]. This advantage positions sub-THz imaging as a multifaceted tool, suitable for bio-imaging [15,16], material analysis [17], and security scanning [18].

Conventional sub-THz imaging typically uses raster scanning, which focuses sub-THz waves onto a minimal focal point and systematically scans the sample pixel by pixel. While raster scanning is capable of producing high-quality images, the cost is the prolonged data acquisition

process. The time-consuming nature of this process is primarily attributed to the use of a two-axis motorized stage in the process. An alternative approach uses a galvanometer with an f-theta lens to improve imaging speed, potentially enabling real-time imaging [19,20]. This approach involves directing the light path to various positions using a galvanometer and realigning it into a single-pixel detector with an f-theta lens. However, using the galvanometer approach entails a trade-off between fields of view (FOV), resolution, and sampling rate. Recently, the use of room temperature array detectors for real-time sub-THz imaging, allowing simultaneous multipixel signal acquisition, is gaining popularity. One notable array detector is the field-effect-transistor (FET) image sensor used in sub-THz imaging cameras [21]. The FET sensor operates by exciting plasma waves in the transistor channel, generating a constant voltage across transistor junctions via nonlinear rectification [22-26], allowing to detect THz electric field in a broad frequency range. However, due to the device parasitics, FET-based cameras usually operate at lower frequencies [26]. The uncooled microbolometer array detector is one of the contenders utilizing image sensors for fast-speed sub-THz imaging. This sensitive detector operates on the principle of detecting thermal variations from received radiation, altering the conductivity of the thermistor material. Therefore, the uncooled microbolometer array detector not only ensures stable image quality but also facilitates real-time imaging.

However, in sub-THz real-time imaging with the array detector, imaging quality is primarily degraded by speckle artifacts with bending and interference profiles. These unexpected artifacts result from the diffraction effect caused by the interaction between coherent sub-THz waves and imaged objects. To mitigate the diffraction-induced artifacts, the optical diffuser is proposed, drawing inspiration from speckle-free imaging in the visible [27] and near-infrared spectra [28]. Optical diffusers primarily scatter incident electromagnetic waves across broader angles. This implementation disrupts wave coherence, leading to the spatial phase independence of the propagated distance, thereby mitigating the diffraction effect. Various optical diffusers in the THz frequency range have been explored by several research groups [29–32]. For instance, 3D-printed phase diffusers made from acrylonitrile butadiene styrene (ABS) have been investigated as random masks to generate pseudo-random patterns for coherent ghost imaging [29]. Utilizing diffuser-aided random patterns to integrate randomized phases allows for image retrieval using iterative or compressed sensing algorithms. Other efforts assess the feasibility of using woodplastic composites to randomize the distribution of materials with various refractive indexes to scatter the waves [30]. Another notable work is the use of air-polymer composite materials with micro-structured air bubbles for scattering the wave over ± 60 degrees from the incident direction, presenting itself as a potential candidate for THz diffusers [31]. Additionally, binary surface reliefs with sub-wavelength features arranged in a pseudo-random pattern have been fabricated as THz diffusers [32], introducing varied sub-cycle delays across different positions through the diffuser. This approach scatters the incident wave into multiple peaks across a range of ± 80 degrees. Nevertheless, these studies primarily focus on the scattering capability of the device, lacking a systematic approach for designing and quantifying its decoherence capability. Moreover, to our knowledge, these diffusers have not yet been explicitly employed in sub-THz real-time imaging, nor have they undergone comprehensive investigation regarding speckle phenomena and practical applications.

In this work, we introduce DaISy, a Diffuser-aided sub-THz real-time Imaging System, utilizing a high-power coherent sub-THz source and an uncooled microbolometer array detector. DaISy incorporates a diffuser made from cost-effective and easily shaped epoxy resin (AB glue, refractive index 1.79 [33]), which breaks coherence and lessens speckle phenomena induced by the coherent wave. To evaluate the speckle phenomena, we introduce a theoretical framework that specifically assesses coherence levels, emphasizing their relation to coherence area and speckle contrast. The diffuser-aided implementation significantly improves imaging quality and resolution, achieving the resolution of 1.428 LP/cm (line pairs per centimeter, i.e. the unit of line pairs, which indicates

the ability to resolve distinct structures within one centimeter). Furthermore, we showcase the practical application of DaISy in security scanning, highlighting its potential as an effective tool.

2. Methods for restraining speckle artifacts in coherent imaging

In sub-THz coherent imaging, the quality of imaging is significantly affected by speckle artifacts, primarily due to notable diffraction effects. These artifacts manifest as speckle patterns when the inherently coherent sub-THz beam interacts with a diffractive interface. Additionally, the mm-level sub-THz wavelength imposes constraints on imaging resolution, limiting the ability to resolve details at a microscopic scale. To mitigate these issues, methods to control the coherent beam have been developed, notably through the use of a THz diffuser coupled with a focusing lens. This method redistributes the phase and amplitude of the wave, effectively shortening the coherence length and disrupting the wavefront uniformity. This, in turn, attenuates the speckle artifacts, leading to improved image quality. Additionally, coherence theory provides a quantitative framework for evaluating speckle phenomena. Through the analysis of speckle contrast associated with the coherence area, the coherence level can be deduced. This analysis of coherence theory also aids in determining the efficacy of the diffuser-lens configuration for speckle evaluation.

2.1. Coherent beam manipulation by focusing lens and designed THz diffuser

In addressing the coherence issues in sub-THz imaging, a focusing lens is adeptly paired with a designed THz diffuser to control the coherent beam. The focusing lens modulates the beam phase profile across varying radii, introducing distinct delays that regulate the convergence of incident waves toward a focal point. This convergence results in the concentration of beam intensity into a small spot, generating a radial dependence in the phase. Subsequently, our efforts have been focused on developing a THz diffuser capable of effectively diminishing wave coherence. The diffuser, characterized by surface irregularities, disperses the coherent beam, playing a crucial role in disrupting its coherence. This is accomplished by scattering the beam at various angles, introducing a random phase distribution across different angles and thereby reducing its uniformity. This mitigation strategy aims to diminish the formation of speckle artifacts.

To attain an effective and maximal random phase distribution, assessing phase variation (PV) $\Delta \phi$ is crucial, as the performance of the diffuser is largely dominated by the degree of PV. The PV measures the level to which the diffuser can alter the phase of the incoming wave, with higher values indicating greater capability for disruption. This capability is quantified as follows

$$\Delta \phi = \frac{2\pi (n - n_0)}{\lambda N_V} \sum_{i=1}^{N_V} \left(H_{\nu_i} - \bar{H} \right)^2$$
(1)

where $n - n_0$ is the change in the refractive index of the medium (in our case, *n* for the diffuser material, $n_0 \approx 1$ for the air), λ is the wavelength of the incident beam passing through the diffuser, N_V is the total number of scanning vertices of the diffuser surface, $V = \{v_i\}$ defines the set comprising all such vertices for $i = 1, ..., N_V$, and \overline{H} is the mean of all heights across these vertices, with H_{v_i} indicating the height of each individual vertex.

In accordance with Eq. (1), the optimal design of the diffuser is characterized by a high refractive index, ensuring maximum efficacy in speckle reduction, which is pivotal for advancing the quality and resolution of coherent sub-THz imaging. Epoxy resin (AB glue), with its high refractive index ($n \approx 1.79$ [33]), cost-effectiveness, malleability, and ease of manufacture, is a prime candidate for prototyping. The high refractive index of AB glue plays a crucial role in enabling more randomized PV, a key element in our diffuser design. Moreover, the potential of such materials can be improved by altering their intrinsic or spatial properties through additives.

The fabrication of AB glue diffusers requires a gradual solidification process, typically taking several hours after mixing. This slow solidification tends to evenly smooth the shape of the AB glue, challenging in achieving randomized PV. Experimentally, we fabricate five sets of AB-glue diffusers and shape them with varying waiting periods after mixing, ranging from 150 to 255 minutes with a 15-minute waiting interval in between (refer to Fig. 1(a) for sample illustrations), to reduce potential errors arising from manual procedures. Moreover, a consistent fabrication temperature of 25 °C is maintained for all diffusers due to the sensitivity of the exothermic nature in the solidification process with AB glue to the ambient temperature (see Supplement 1).



Fig. 1. Illustrations of Fig. 1(a) AB-glue diffusers with varying waiting periods after mixing, ranging from 150 to 255 minutes with a 15-minute waiting interval in between; Fig. 1(b) phase variations of five sets of diffusers with varying waiting times for shaping after mixing where different fabricating set of diffusers are indicated using specific colours.

For the evaluation of the PV of each diffuser after fabrication, the blue-light 3D Scanner (AutoScan Inspec, SHINNING 3D) is used to capture the height information of the diffuser surface vertices with an accuracy below 10 µm. Then, the PV of each diffuser is quantified, as shown in Fig. 1(b), indicating the upward trend. This upward trend in PV corresponds to increased surface roughness, resulting from higher viscosity due to longer elapsed times before shaping. The increased surface roughness breaks the uniformity of coherent waves by scattering them, which in turn introduces PV, randomizes wavefront, and reduces coherent interference. Note that a saturation point exists in PV, beyond which further waiting does not lead to considerable improvements. This saturation point is reached when the AB glue reaches an equilibrium in its solidification process, leading to minimal changes in surface texture. Despite the limitations of our prototyping AB glue diffusers, we next provide the adapted coherence theory related to PV values for speckle evaluation to assess the coherence level of the coherent beam manipulation by the THz diffuser with a focusing lens.

2.2. Coherence theory for speckle evaluation

Effective mitigation of speckle artifacts is anticipated by manipulating the coherent beam through a focusing lens and a specially designed THz diffuser. Such manipulation of the coherent beam leads to alterations in speckle phenomena, which can be quantitatively evaluated using the concept of speckle contrast derived from optical coherence theory [34,35]. For simplicity, we first introduce coherence theory in the context of a diffuser-only configuration to derive the speckle contrast. Then, an adapted coherence theory, incorporating both the diffuser and the focusing

lens, is presented. This adapted theory allows us to assess the effectiveness of these methods in reducing speckle artifacts, thereby improving image quality in coherent imaging.

2.2.1. Analysis with diffuser-only configuration

Beginning our analysis with a diffuser-only configuration, we explore the impact of the THz diffuser on speckle phenomena through coherence theory [34,35]. This analysis specifically evaluates the impact of the diffuser on the coherence of the beam, providing a clear basis for understanding the variations of speckle phenomena.

Assuming a lossless THz diffuser with a stationary and steady random phase profile, we consider the scenario where the diffuser is in a rotating motion for time-varying phase alterations. The THz field interacting with this rotating diffuser can be mathematically expressed as

$$\mathbf{a}(\alpha,\beta;t) = \mathbf{a}_0 e^{j\phi_0(\alpha,\beta)} e^{j\phi_d(\alpha-\nu t,\beta)}$$
(2)

where \mathbf{a}_0 is the constant amplitude, $\phi_0(\alpha, \beta)$ represents the phase of incident waves at any position (α, β) in the given plane with two α, β directions, and $\phi_d(\alpha - vt, \beta)$ refers to the phase of the THz diffuser with a moving speed *v* over time *t*. To evaluate the coherence of the THz field after passing through a diffuser, mutual coherence Γ_{12} is employed, examining the correlation between two distinct positions within an observation plane,

$$\boldsymbol{\Gamma}_{12}(\alpha_1,\beta_1,\alpha_2,\beta_2;\Delta t) = |\mathbf{a}_0|^2 \langle e^{j\phi_d(\alpha_1 - \nu t,\beta_1)} e^{-j\phi_d(\alpha_2 - \nu t - \nu\Delta t,\beta_2)} \rangle \tag{3}$$

where (α_1, β_1) and (α_2, β_2) are two different positions on the same plane, Δt represents a small time difference, and $\langle \cdot \rangle$ denotes as an infinite time average. Given that speckle phenomena are fundamentally determined by the phase of mutual coherence, the latter time average term of Eq. (3) crucially describes the coherence level. Since the diffuser follows a random phase process ϕ_d , characterized by Gaussian distribution with zero mean and statistically stationary, the coherence level γ_{12} is derived from the relationship of above average and the characteristic function (details in Thm. A.1 of Appendix A)

$$\gamma_{12}(\Delta\alpha,\Delta\beta;\Delta t) = \langle e^{j\phi_d(\alpha_1 - \nu t\beta_1)} e^{-j\phi_d(\alpha_2 - \nu t - \nu\Delta t\beta_2)} \rangle \underline{\text{Thm. A.1}} e^{-\sigma_\phi^2 [1 - \mu_\phi(\Delta\alpha + \nu\Delta t,\Delta\beta)]}$$
(4)

where $\Delta \alpha = \alpha_1 - \alpha_2$, $\Delta \beta = \beta_1 - \beta_2$, σ_{ϕ} refers to the standard deviation of the diffuser phase, and μ_{ϕ} represents the normalized autocorrelation function of the phase. Furthermore, this autocorrelation function μ_{ϕ} is modeled as a Gaussian shape for subsequent analysis

$$\mu_{\phi}(\Delta\alpha, \Delta\beta) = e^{-\frac{\Delta\alpha^2 + \Delta\beta^2}{r_{\phi}^2}}$$
(5)

where r_{ϕ} is the correlation radius of the phase. Here, the correlation radius of the phase r_{ϕ} indicates the degree of autocorrelation in PV caused by the diffuser. A higher degree of randomness in the diffuser typically results in a smaller r_{ϕ} . Conversely, greater smoothness in the diffuser surface is associated with a larger r_{ϕ} . Note that the slow solidification process leads to a progressive smoothing of the surface in the diffuser over the solidification period. This smoothing effect increases the autocorrelation value, indicating a larger r_{ϕ} .

Considering the transient characteristics of the observation plane, the analysis of speckle phenomena is predominantly governed by the spatial coherence level. In this scenario, temporal coherence is rendered negligible, i.e. $\Delta t = 0$, thereby focusing the assessment solely on spatial aspects of coherence in relation to speckle phenomena. Following Eqs. (4), (5), the spatial

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coherence level can be reformulated as follows

$$\gamma_{12}(\Delta\alpha,\Delta\beta;0) = e^{-\sigma_{\phi}^{2} \left(1-e^{-\frac{\Delta\alpha^{2}+\Delta\beta^{2}}{r_{\phi}^{2}}}\right)}.$$
(6)

Then, to determine the spatial coherence level over an infinite area, integration of $\gamma_{12}(\Delta \alpha, \Delta \beta; 0)$ across the variable $(\Delta \alpha, \Delta \beta)$ represents the coherence area. However, this direct integration may not converge due to monotonically non-decreasing integrand over an infinite interval. To address this issue, a renormalization process is employed, ensuring that the integral maintains unity at its origin. This process is achieved by adjusting the term $e^{-\sigma_{\phi}^2}$ from $\gamma_{12}(\Delta \alpha, \Delta \beta; 0)$. Specifically, the key adjustment is the division of the integral by the factor $(1 - e^{-\sigma_{\phi}^2})$ to ensure the unity value at the origin. Therefore, the coherence area, following these adjustments, can be represented

$$\mathcal{A}_{c} = \iint_{-\infty}^{\infty} \left[\frac{\gamma_{12}(\Delta\alpha, \Delta\beta; 0) - \gamma_{12}(\infty, \infty; 0)}{1 - \gamma_{12}(\infty, \infty; 0)} \right] d\Delta\alpha d\Delta\beta$$
$$= \frac{e^{-\sigma_{\phi}^{2}}}{1 - e^{-\sigma_{\phi}^{2}}} \iint_{-\infty}^{\infty} \left(e^{\sigma_{\phi}^{2}e^{-\frac{\Delta\alpha^{2} + \Delta\beta^{2}}{r_{\phi}^{2}}} - 1} \right) d\Delta\alpha d\Delta\beta.$$
(7)

After determining the coherence area, the speckle contrast can be derived to evaluate the speckle phenomena. If the diffuser is uniformly illuminated over a constant area \mathcal{A}_D , this leads to the generation of multiple coherence areas \mathcal{A}_c on its surface. Each of these coherence areas \mathcal{A}_c contributes an independent speckle intensity pattern to the observation plane. Then, the speckle contrast can be approximately expressed as

$$C \approx \begin{cases} 1 & \text{if } \mathcal{R}_c \ge \mathcal{R}_D \\ \left(\frac{\mathcal{R}_c}{\mathcal{R}_D}\right)^{\frac{1}{2}} & \text{if } \mathcal{R}_c < \mathcal{R}_D \end{cases}$$
(8)

where \mathcal{A}_D represents the constant area illuminated on the diffuser. With the coherence area of each diffuser in Fig. 2(a), the speckle contrast value can be calculated by Eq. (8) for each diffuser shaped with different waiting times as shown in Fig. 2(b). As previously mentioned, the diffuser with longer waiting times exhibits a greater PV and a smaller correlation radius r_{ϕ} of the phase. Following that, these diffusers manifest a reduced coherence level, resulting in a lower speckle contrast value. Specifically, upon illuminating 1 m² area with a coherent beam, the minimal speckle contrast value is 0.4563, as indicated in Fig. 2(b). We choose the diffuser associated with this minimal value to break the sub-THz source coherence level externally, with the aim of achieving incoherent illuminated sub-THz imaging. Nevertheless, in our implementations using a single THz diffuser, the resulting imaging is still affected by a certain degree of wave diffraction. This limitation arises from the saturation point in PV, as discussed in 2.1.

2.2.2. Adapted analysis with diffuser-lens configuration

Expanding upon the initial insights from the diffuser-only configuration in 2.2.1, we now explore an adapted analysis that integrates both the THz diffuser and the focusing lens within the coherence theory framework. In this comprehensive analysis, the interaction between the diffuser and the lens is examined to understand how their synergistic effect alters spatial coherence. Here, the lens not only focuses the beam but also modifies its phase characteristics, which, when combined with the random phase alterations induced by the diffuser, could result in a more pronounced reduction in speckle artifacts. The coherence theory is adapted accordingly to account for these manipulations, providing a more robust framework for evaluating the effectiveness of the diffuser-lens combination in speckle mitigation. Research Article

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Fig. 2. Illustrations of Fig. 2(a) coherence area of five sets of diffusers derived by Eq. (7); Fig. 2(b) speckle contrast values of five sets of diffusers calculated from Fig. 2(a) and derived by Eq. (8); where different fabricating set of diffusers are indicated using specific colours.

Assuming the initial beam has a uniform phase at the same plane and passes through a thin focusing lens with a focal length f_l , the diffuser is positioned at the focus spot of this lens. By applying the Fresnel diffraction equation [36], the mathematical description of the optical field of the beam on the surface of the diffuser is as follows

$$\mathbf{U}(\alpha,\beta) = \frac{e^{jkf_l}e^{j\frac{k}{2f_l}(\alpha^2+\beta^2)}}{j\lambda f_l} \iint_{-\infty}^{\infty} \left[\mathbf{U}_0(x,y)e^{j\frac{k}{2f_l}(x^2+y^2)}e^{-j\frac{2\pi}{\lambda f_l}(\alpha x+\beta y)} \right] \,\mathrm{d}x\mathrm{d}y \tag{9}$$

where *k* represents the wavelength number, f_l refers to the focal length of the thin focusing lens, (x, y) represents a point on the initial plane of the light source, $\mathbf{U}_0(x, y)$ signifies the optical field at starting plane, and (α, β) represents the point on the plane situated at focal spot position *F*. Since $\mathbf{U}(\alpha, \beta)$ is the optical field before the incident to the diffuser, Eq. (2) can be rewritten as

$$\mathbf{a}(\alpha,\beta;t) = \mathbf{U}(\alpha,\beta)e^{j\phi_d(\alpha-\nu t,\beta)}.$$
(10)

Then, the coherence level in Eq. (4) can be reformulated as

$$\gamma_{12}(\Delta\alpha, \Delta\beta, \alpha_2, \beta_2; \Delta t) = e^{-\sigma_{\phi}^2 [1 - \mu_{\phi}(\Delta\alpha + \nu\Delta t, \Delta\beta)]} e^{j\frac{k}{2f_l} [\Delta\alpha(\Delta\alpha + 2\alpha_2) + \Delta\beta(\Delta\beta + 2\beta_2)]} \iint_{-\infty}^{\infty} e^{-j\frac{2\pi}{M_l} (x\Delta\alpha + \nu\Delta\beta)} dxdy$$
(11)

where $\Delta \alpha = \alpha_1 - \alpha_2$, $\Delta \beta = \beta_1 - \beta_2$. Considering the spatial coherence level with $\Delta t = 0$, and (α_2, β_2) is situated at the center of the beam, the adapted coherence area in Eq. (7) can be derived as

$$\tilde{\mathcal{A}}_{c} = \iint_{-\infty}^{\infty} \frac{e^{-\sigma_{\phi}^{2} + \phi_{F}(\Delta\alpha, \Delta\beta)}}{1 - e^{-\sigma_{\phi}^{2} + \phi_{F}(\Delta\alpha, \Delta\beta)}} \left\{ e^{\left[\sigma_{\phi}^{2} e^{-\frac{\Delta\alpha^{2} + \Delta\beta^{2}}{r_{\phi}^{2}}} + \phi_{F}(\Delta\alpha, \Delta\beta)\right]} - 1 \right\} d\Delta\alpha d\Delta\beta$$
(12)

where $\phi_F(\Delta \alpha, \Delta \beta)$ refers to the contribution of coherence area from the focusing lens

$$\phi_F(\Delta\alpha,\Delta\beta) = \iint_{-\infty}^{\infty} \left[e^{-j\frac{k}{2l_l}(\Delta\alpha^2 + \Delta\beta^2) + j\frac{2\pi}{M_l}(x\Delta\alpha + y\Delta\beta)} \right] \, \mathrm{d}x\mathrm{d}y. \tag{13}$$

After wave propagation through the diffuser-lens configuration, the adapted coherence area can be adjusted in various configurations associated with Eq. (12). This demonstrates the potential for declining the coherence area when using a fixed phase-variation diffuser. Moreover, since the index of $\phi_F(\Delta \alpha, \Delta \beta)$ is divided by the focal length f_i , a larger value of f_i has a more subtle effect on the coherence area, while a shorter focal length amplifies this effect. For example, when the maximum PV is 4.12 using a THz focusing lens ($f_i = 3$ cm), the speckle contrast can be reduced from 0.4563 to 0.0211. This diffuser-lens configuration suggests a solution to the challenge of shaping AB-glue diffusers to achieve imaging without significant distortion and a subsequent reduction in speckle artifacts.

3. Diffuser-aided sub-THz imaging system (DalSy) with results and discussions

The Diffuser-aided sub-THz Imaging System (DaISy) is configured with specified distances between each component as depicted in Fig. 3. From right to left in the schematic diagram, the coherent sub-THz source consists of a microwave signal generator (SMB100A, Rohde & Schwarz) and a frequency multiplier (WR-5.1, Virginia Diodes) with a conical horn antenna (WR-5.1, Virginia Diodes) optimized for wave generation and propagation. This assembly generates directional coherent radiation at 200.4 GHz by configuring the microwave signal generator to 16.7 GHz and amplifying it twelvefold through the frequency multiplier. A 2-inch plano-convex THz lens (focal length: $f_l = 3$ cm) is introduced between the THz diffuser and the horn antenna, where the THz diffuser is placed at the focal point of this THz lens. Here, this THz lens serves to initially redistribute the phase of coherent waves, thereby amplifying the ability of the diffuser to break the coherence of incoming waves. All lenses employed in our DaISy, made of polypropylene (PP), are self-manufactured using computer numerical control (CNC) machinery. The THz diffuser is chosen with the highest PV value (PV = 4.12) to suppress the coherence level of the sub-THz radiation. This suppression correlates with a decrease in speckle artifacts, thereby improving the clarity and quality of the captured images. The THz diffuser is mounted on a rotation motor (\mathcal{R}) that operates at a speed of 1000 revolutions per minute (rpm). This rotating diffuser allows the incoming coherent wave to pass through varying thicknesses of the diffuser in a short time, effectively converting it into incoherent waves.



Fig. 3. Schematic diagram of the Diffuser-aided sub-THz Imaging System (DaISy).

As the incoherent sub-THz beam propagates through the THz diffuser, a 2-inch plano-convex THz lens ($f_l = 10 \text{ cm}$) is positioned to resize and efficiently collect the sub-THz beam, including the scattering components. Subsequently, the propagated sub-THz beam covers the whole area of the object being imaged. Following the object, a 4-inch plano-convex THz lens ($f_l = 17 \text{ cm}$) is implemented to focus the sub-THz beam onto the focal plane array of the THz camera for imaging. Then, the image is captured using an uncooled microbolometre array-detector THz camera (MICROXCAM-384i-THz, INO) with a THz objective lens (F/0.7, INO; $f_l = 4.4 \text{ cm}$). As this camera is highly sensitive to thermal variations, we attach a 0.1-mm-thick paper on top of the THz objective lens as the filter to attenuate environmental heat/light perturbations. All imaging results obtained from the THz camera take the normalization process from their raw files by the programming language MATLAB_R2023b[®] performed on macOS Sonoma 14.2 with an Apple M1 Max Chip and 64 GB Memory.

As elaborated in 2, solely using a diffuser does not suffice to meet the desired DaISy performance criteria. To demonstrate this, experiments are conducted under three different configurations: without both a diffuser and a focusing lens, using only a diffuser, and combining both a diffuser and a focusing lens. Initially, we explore the formation of speckle patterns with Gaussian sub-THz beam illumination, as depicted in Fig. 4. In the first scenario (4(a)), where neither the diffuser nor the focusing lens is used, we observe a speckle contrast of 0.409, indicating a high level of speckle artifacts due to the nature of coherence imaging. In the second configuration, where only the diffuser is employed (4(a)), there is a noticeable decrease in speckle contrast to 0.255. This decrease demonstrates the effectiveness of the diffuser in altering the coherence of the beam, thereby influencing the speckle patterns. A further improvement is seen in the third configuration (4(b)) with the addition of the focusing lens to the diffuser. Here, the speckle contrast is further reduced to 0.155, showcasing the improved capability of this combined configuration in reducing speckle artifacts. The decreasing speckle contrast values across our configurations demonstrate the effectiveness of both the diffuser and lens in breaking beam coherence, directly improving image clarity. This consistent trend highlights the significant role each component plays in achieving higher image quality and moving towards speckle-free imaging.



Fig. 4. Without Diffuser and Lens

We now proceed to evaluate the effectiveness of speckle reduction in realistic imaging scenarios using our DaISy on a "Y"-shaped 3D-printed test object, as depicted in Fig. 5(a). The strategic selection of a "Y"-shaped object, with its branching structure with varying angles and contours, makes it ideal for evaluating speckle phenomena across different tilt directions. First, the sub-THz imaging result without the diffuser, shown in Fig. 5(b), reveals that the test object is barely distinguishable, with the image quality significantly impaired by speckle artifacts. This highlights the limitations of the system without any speckle mitigation components. When only the diffuser is employed, as seen in Fig. 5(c), the "Y" shape of the test object becomes somewhat discernible, yet the image suffers from blurry and lack of clarity. Additionally, the edges of the object are distorted, indicating the persistence of diffraction effects. The most significant

improvement is observed in Fig. 5(d) with the complete configuration (3), incorporating both the diffuser and the focusing lens. This configuration markedly improves image contrast, making the edges of the object easily identifiable. The clarity achieved in this image starkly contrasts with the previous results, especially compared to the diffuser-only configuration in Fig. 5(c). This comparison underscores the effectiveness of the combined use in achieving speckle-free imaging and delineating finer details.



Fig. 5. Illustrations of Fig. 5(a) the "Y"-shaped 3D-printed test object for various experimental configurations: Fig. 5(b) without diffuser and focusing lens; Fig. 5(c) with diffuser only (no focusing lens); Fig. 5(d) with diffuser and focusing lens.

To quantify the improved image quality from our DaISy system, we employ a comprehensive set of quality metrics outlined in Table 1. Table 1 showcases the performance of Fig. 5(b)-5(d) by our DaISy across different configurations: without both a diffuser and a focusing lens, using only a diffuser, and combining both a diffuser and a focusing lens. These metrics assess image quality from two perspectives: full-reference quality metrics and no-reference quality metrics. For full-reference quality metrics, we compare the acquired images against an ideal reference image, which is derived from the 3D printing file of the "Y"-shaped object. All full reference quality metrics, namely the peak signal-to-noise ratio (PSNR), the structural similarity index measure (SSIM), and the mean-squared error (MSE), show progressive improvements. In detail, PSNR jumps significantly from 2.3095 to 7.4017 with the full DaISy setup, indicating a cleaner signal with less noise. SSIM increases from 0.2256 to 0.5858, reflecting improved clarity and structural accuracy. MSE decreases from 0.5876 to 0.1819, pointing to a lower error between the acquired and reference images. Additionally, in a complementary manner, we incorporate no-reference quality metrics, namely the blind/referenceless image spatial quality evaluator (BRISQUE) and the natural image quality evaluator (NIQE), to evaluate the images without a reference image. BRISQUE scores decrease from 66.9749 to 63.4722, denoting images that appear more natural and less distorted. NIQE scores also improve from 6.5987 to 6.2490, suggesting a quality closer to what the human eye perceives as natural. By combining these metrics, we offer a comprehensive evaluation of image quality, highlighting the capability of DaISy to produce detailed and clear images of the "Y"-shaped specimen without speckle artifacts. For a detailed explanation of the quality metrics used in our work, please refer to Supplement 1 [37–41].

Next, for evaluating imaging resolution with DaISy, we utilize the scaled USAF-1951 resolution test, a standard benchmark in imaging system assessment. As illustrated in Fig. 6(a), this test features line pairs varying from 11 mm (top) to 7 mm (bottom), providing a comprehensive test of the resolving capabilities for DaISy. For the first configuration, the imaging results without using a diffuser or a focusing lens, shown in Fig. 6(b), display significant distortion. The larger line pairs, measuring 11 mm, appear blurred, achieving a resolution of only 0.9 line pairs per centimeter (LP/cm). A considerable improvement in resolution is observed when employing only the diffuser, as depicted in Fig. 6(c). In this configuration, the system is able to resolve line pairs down to 9 mm, translating to a resolution of 1.11 LP/cm. However, it falls short of distinguishing the finer details of smaller line pairs, indicating the need for further improvement in the resolving

Table 1. Comparison metrics for the image quality of Fig. 5(b)-5(d) of the "Y"-shaped test object by the full-reference perspective: peak signal-to-noise ratio (PSNR), structural similarity index measure (SSIM), and mean-squared error (MSE), as well as the no-reference perspective: blind/referenceless image spatial quality evaluator (BRISQUE) and naturalness image quality evaluator (NIQE) where ↑ (↓): higher (lower) is better.

		Without Diffuser	With Diffuser Only	With Diffuser and Lens
Full-Reference	PSNR (†)	2.3095	4.0357	7.4017
	SSIM (†)	0.2256	0.3844	0.5858
	MSE (\downarrow)	0.5876	0.3948	0.1819
No-Reference	BRISQUE (\downarrow)	66.9749	65.4817	63.4722
	NIQE (\downarrow)	6.5987	6.5692	6.2490

ability. The most significant advancement is achieved with the integration of both the diffuser and focusing lens, as shown in Fig. 6(d). This complete configuration enables DaISy to perform at its optimal capacity, successfully resolving line pairs as small as 7 mm. This corresponds to an improved resolution of 1.428 LP/cm, clearly demonstrating the improved capabilities in achieving speckle-free imaging with superior resolution.



(a) Resolution Test Object (b) Withou

(b) Without Diffuser

(c) With Diffuser Only

er Only (d) With Diffuser and Lens

Fig. 6. Illustrations of Fig. 6(a) scale USAF-1951 resolution test object, where the scale object displaying resolution ranging from 0.9 LP/cm to 1.428 LP/cm, fabricated by a gold stamping printing process, for various experimental configurations: Fig. 6(b) without diffuser and focusing lens; Fig. 6(c) with diffuser only (no focusing lens); Fig. 6(d) with diffuser and focusing lens.

Last, the capabilities of our DaISy extend beyond laboratory testing and find practical applications in real-world scenarios. Particularly in the scenario of security scanning, sub-THz imaging stands out due to its unique ability to peer inside concealed objects with exceptional precision. To illustrate its practical utility, we conduct a demonstration where a small sculpture knife is concealed in the pocket of a standard nylon jacket, as exemplified in Fig. 7(a). The optical image of this concealed sculpture knife is shown in Fig. 7(b), akin to that of a pen. Leveraging the DaISy, we perform sub-THz imaging of the jacket, and the results, displayed in Fig. 7(c), are nothing short of impressive. The semblance of the sculpture knife is easy to identify and profile despite its diminutive size of approximately 5 mm. Remarkably, even when concealed within the fabric of the jacket, our system offers unparalleled visibility. These outcomes underscore the

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potential of DaISy as a valuable tool in security scanning and inspections, where the precise detection of concealed items is of paramount importance.



Fig. 7. DaISy demo in security scanning application: Fig. 7(a) the concealed sculpture knife within a nylon jacket pocket; Fig. 7(b) the isolated sculpture knife; Fig. 7(c) visualization of the sculpture knife using our DaISy with diffuser and focusing lens.

4. Conclusion

The development and implementation of DaISy represent a major advancement in addressing the speckle artifacts in coherent sub-THz imaging. At its core, this advancement is driven by integrating a specially designed THz diffuser, made from easily malleable and cost-effective epoxy resin (AB glue), and complemented by a focusing lens. This strategic combination effectively breaks the beam coherence, significantly reducing speckle artifacts that arise from the undesired diffraction phenomenon. In this work, we establish a theoretical framework in coherence theory to facilitate the design and validation of THz components. This framework enables a systematic and quantitative assessment of speckle phenomena associated with different coherence levels. Initially, we developed this framework in a configuration employing only a diffuser to analyze speckle contrast. Subsequently, we expand this coherence framework to incorporate the wave propagation behavior resulting from the introduction of a diffuser-lens configuration. These comprehensive analyses aim to evaluate the efficacy of speckle mitigation, revealing significant enhancements in both image quality and resolution. The achievement of a 1.428 LP/cm in resolution is a testament to the efficacy of this approach, pushing the boundaries of a few-cycle resolution in sub-THz imaging. Moreover, the practical application of DaISy, particularly demonstrated in security scanning, highlights the versatile potential of sub-THz waves in various fields. The ability to discern concealed objects with improved clarity and precision underlines the value of DaISy in real-world scenarios, opening doors to its use in diverse areas ranging from non-invasive sensing and imaging to industrial inspection to bioinformatics.

However, one of the limitations of the current demonstrated system is it can only capture the spatial information of objects, lacking the capacity to collect multi-dimensional information for

further analysis. Recent advancements in machine learning techniques have shown great promise in extracting phase information through amplitude information [42–45]. By incorporating data-driven methodologies within the DaISy architecture, it is expected to have real-time, highly precise, cost-effective, and low-complexity THz imaging systems in the near future. This advancement holds great promise for expanding the application scopes of THz imaging, akin to its neighboring electromagnetic wave bands.

A. Derivation of Eq. (4)

Theorem A.1. If ϕ is a random variable of a Gaussian (normal) distribution $\phi \sim \mathcal{N}(\mu_{\phi} = 0, \sigma_{\phi}^2)$ with zero mean μ_{ϕ} and standard deviation σ_{ϕ} (variance σ_{ϕ}^2), there exists

$$\mathbb{E}\{e^{j\Delta\phi}\} = \langle e^{j\Delta\phi}\rangle = \overline{e^{j\Delta\phi}} = e^{-\sigma_{\phi}^{2}[1-\mu_{\phi}(\Delta\alpha,\Delta\beta)]}$$

Proof. Since ϕ is a Gaussian (normal) random variable $\phi \sim \mathcal{N}(\mu_{\phi} = 0, \sigma_{\phi}^2)$, its Gaussian probability density function (PDF) can be formulated as

$$p(\phi) = \frac{1}{\sqrt{2\pi\sigma_{\phi}^2}} e^{-\frac{(\phi-\mu_{\phi})^2}{2\sigma_{\phi}^2}} \underline{\mu_{\phi}} = 0 \frac{1}{\sqrt{2\pi\sigma_{\phi}^2}} e^{-\frac{\phi^2}{2\sigma_{\phi}^2}}.$$

Note that $\Delta \phi$ is also a Gaussian random variable.

The characteristic function of above PDF $p(\phi)$ is the complex conjugate of the continuous Fourier transform of $p(\phi)$

$$\varphi_{\phi} = \mathbb{E}\{e^{j\phi}\} = \langle e^{j\phi} \rangle = \overline{e^{j\phi}} = \frac{1}{\sqrt{2\pi\sigma_{\phi}^2}} \int_{-\infty}^{\infty} \left[e^{-\frac{(\phi-\mu_{\phi})^2}{2\sigma_{\phi}^2}} e^{j\phi} \right] d\phi$$
$$= \frac{1}{\sqrt{2\pi\sigma_{\phi}^2}} \int_{-\infty}^{\infty} \left\{ e^{-\frac{1}{2\sigma_{\phi}^2} \left[\phi - (\mu_{\phi} + j\sigma_{\phi}^2) \right]^2 - \frac{1}{2}\sigma_{\phi}^2 + j\mu_{\phi}} \right\} d\phi$$
$$= e^{-\frac{1}{2}\sigma_{\phi}^2 + j\mu_{\phi}} \frac{1}{\sqrt{2\pi\sigma_{\phi}^2}} \int_{-\infty}^{\infty} \left\{ e^{-\frac{1}{2\sigma_{\phi}^2} \left[\phi - (\mu_{\phi} + j\sigma_{\phi}^2) \right]^2} \right\} d\phi$$
$$\underbrace{\text{by Gaussian integral}}_{e^{-\frac{1}{2}\sigma_{\phi}^2 + j\mu_{\phi}}} \mu_{\phi} = 0 e^{-\frac{1}{2}\sigma_{\phi}^2}.$$

Then, there exists

$$\varphi_{\Delta\phi} = \mathbb{E}\{e^{j\Delta\phi}\} = e^{-\frac{1}{2}\sigma_{\Delta\phi}^2} = e^{-\sigma_{\phi}^2[1-\mu_{\phi}(\Delta\alpha,\Delta\beta)]}$$

where

$$\sigma_{\Delta\phi}^2 = \mathbb{E}\{(\Delta\phi)^2\} = \mathbb{E}\{\phi_1^2\} + \mathbb{E}\{\phi_2^2\} - 2\mathbb{E}\{\phi_1\phi_2\} = \sigma_{\phi}^2 + \sigma_{\phi}^2 - 2\sigma_{\phi}^2\mu_{\phi}(\Delta\alpha, \Delta\beta)$$

with

$$\begin{split} \mathbb{E}\{\phi_1\phi_2\} &= \mathbb{E}\{\phi_1(\alpha,\beta)\phi_2(\alpha+\Delta\alpha,\beta+\Delta\beta)\}\\ &= \mathbb{E}\{\phi_1(\alpha,\beta)\phi_2(\alpha,\beta)\}\mathbb{E}\{\phi_2(\Delta\alpha,\Delta\beta)\}\\ &= \sigma_{\phi}^2\mu_{\phi}(\Delta\alpha,\Delta\beta), \end{split}$$

which is the autocorrelation function

$$\mu_{\phi}(\Delta \alpha, \Delta \beta) = \frac{\mathbb{E}\{\phi_1(\alpha, \beta)\phi_2(\alpha + \Delta \alpha, \beta + \Delta \beta)\}}{\sigma_{\phi}^2}$$

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Supplemental document. See Supplement 1 for supporting content.

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