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An augmented Lagrangian method for solving total variation (TV)-based image registration model

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Abstract

Variational methods for image registration basically involve a regularizer to ensure that the resulting well-posed problem admits a solution. Different choices of regularizers lead to different deformations. On one hand, the conventional regularizers, such as the elastic, diffusion and curvature regularizers, are able to generate globally smooth deformations and generally useful for many applications. On the other hand, these regularizers become poor in some applications where discontinuities or steep gradients in the deformations are required. As is well-known, the total (TV) variation regularizer is more appropriate to preserve discontinuities of the deformations. However, it is difficult in developing an efficient numerical method to ensure that numerical solutions satisfy this requirement because of the nondifferentiability and non-linearity of the TV regularizer. In this work we focus on computational challenges arising in approximately solving TV-based image registration model. Motivated by many efficient numerical algorithms in image restoration, we propose to use augmented Lagrangian method (ALM). At each iteration, the computation of our ALM requires to solve two subproblems. On one hand for the first subproblem, it is impossible to obtain exact solution. On the other hand for the second subproblem, it has a closed-form solution. To this end, we propose an efficient nonlinear multigrid (NMG) method to obtain an approximate solution to the first subproblem. Numerical results on real medical images not only confirm that our proposed ALM is more computationally efficient than some existing methods, but also that the proposed ALM delivers the accurate registration results with the desired property of the constructed deformations in a reasonable number of iterations.

Keywords

Image registration, augmented Lagrangian method, nonlinear multigrid method, total variation regularization

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Introduction

One of important tasks in image analysis is image registration. Generally speaking, it is the process of matching two or more images of the same or similar object obtained from different times, perspectives, and/or imaging sensors. This process can be done mathematically by computing a spatial geometric transformation of deformations (also known as displacement fields) that maps each point in one image onto a corresponding point in the other image with an *optimal* or *meaningful* manner. Image registration has played an important role in several areas of applications. Especially in medical applications, for example, it has been used routinely in medical diagnosis, treatment guidance and monitoring for providing complementary

information. A good survey of the medical applications can be seen in literature^{1–4} and the references therein.

Variational methods for image registration have been actively and extensively studied and applied in the field of image analysis. The main idea is to find spatial correspondences between two given images, a

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so-called reference image $R:\Omega\subset\mathbb{R}^2\to V\subset\mathbb{R}$ and a so-called template image $T:\Omega\subset\mathbb{R}^2\to V\subset\mathbb{R}$, where the image domain Ω is assumed to be a rectangle. This is usually done by finding an optimal deformation $u:\mathbb{R}^2\to\mathbb{R}^2, u:x\mapsto u(x)=(u_1(x),u_2(x))^{\top}$, such that the transformed version of the template image $T_u(x)=T(x+u(x))$ and the reference image R are spatially matched, according to an image-to-image dissimilarity measure, $\mathcal{D}(u)$. Without loss of generality, this work assumes that $\Omega=[0,1]^2\subset\mathbb{R}^2$ and V=[0,1] for 2D gray intensity images. Note that the choice of Ω is somewhat arbitrary. The unit square $\Omega=[0,1]^2$ is adopted and used in all numerical sections throughout this work in order to make the performance comparison of the proposed numerical method with that of literature.

If the image intensities of the given images R and T are comparable, one may have various choices for \mathcal{D} . Probably the most popular choice for the dissimilarity measure is provided by the so-called *sum of squared differences* (SSD)

$$\mathcal{D}(\boldsymbol{u}) = \frac{1}{2} \int_{\Omega} (T_{\boldsymbol{u}}(\mathbf{x}) - R(\mathbf{x}))^2 d\mathbf{x}$$

The registration task is then to solve the minimization problem

$$\min_{\mathbf{u}} \{ \mathcal{D}(\mathbf{u}) \} \tag{1}$$

where u is searched over a set of admissible functions \mathcal{U} minimizing \mathcal{D} . As is well-known, the minimization of \mathcal{D} does not have a unique minimizer and it becomes necessary to impose a constraint on the solution u via a regularizer \mathcal{R} . By modifying (1), the desired deformation u is a minimizer of the variational problem

$$\min_{\mathbf{u}} \{ \mathcal{J}_{\alpha}(\mathbf{u}) = \mathcal{D}(\mathbf{u}) + \alpha \mathcal{R}(\mathbf{u}) \}$$
 (2)

where $\alpha > 0$ is a positive constant that compromises the quality of the similarity between T_u and R, measured by \mathcal{D} , and the level of penalty for unwanted deformations, measured by \mathcal{R} .

In this work, we focus on the regularizer of the form

$$\mathcal{R}(\boldsymbol{u}) = \sum_{l=1}^{2} \mathcal{R}^{\text{TV}}(u_l)$$
 (3)

where

$$\mathcal{R}^{\text{TV}}(u_l) = \int_{\Omega} |\nabla u_l| d\mathbf{x} = \int_{\Omega} \sqrt{u_{l,x}^2 + u_{l,y}^2} d\mathbf{x}$$

with $u_{l,x} = \frac{\partial u_l}{\partial x}$ and $u_{l,y} = \frac{\partial u_l}{\partial y}$ to ensure that the constructed deformation \boldsymbol{u} is unique and preserves discontinuities of the deformations. This term is known as the total variation (TV) regularizer.^{5–7} In contrast to other traditional regularizers generating globally smooth deformations, e.g. elastic⁸ diffusion⁹ and curvature regularizers^{10,11} the TV regularizer is able to produces locally non-smooth deformations, which are required in matching several moved objects or partially occluded objects in medical applications, particularly at organ boundaries during the breathing induced organ motion.

In order to get a numerical solution of the variational problem (2), the standard gradient descent method can be applied. We first embed the associated Euler-Lagrange (EL) equation of (2) into a dynamic equation and drive it to a steady state. This yields the explicit scheme as given by

$$\begin{cases}
\frac{u_{1}^{[k+1]} - u_{1}^{[k]}}{\tau} = \alpha \nabla \cdot \left(\frac{\nabla u_{1,x}^{[k]}}{\sqrt{(u_{1,x}^{[k]})^{2} + (u_{1,y}^{[k]})^{2} + \beta}} \right) - f_{1}(\boldsymbol{u}^{[k]}), \\
\frac{u_{2}^{[k+1]} - u_{2}^{[k]}}{\tau} = \alpha \nabla \cdot \left(\frac{\nabla u_{2}^{[k]}}{\sqrt{(u_{2,x}^{[k]})^{2} + (u_{2,y}^{[k]})^{2} + \beta}} \right) - f_{2}(\boldsymbol{u}^{[k]}),
\end{cases}$$
(4)

where $f_l(\mathbf{u}^{[k]}) = (T_{\mathbf{u}^{[k]}} - R)\partial_{u_l}T_{\mathbf{u}^{[k]}}, k = 0, 1, 2, \dots$ is the time step, $\tau > 0$ is the step size, and $\beta > 0$ is a small real parameter to avoid zero division; see more details in literature. ^{12–14} This numerical scheme is easy to implement, but very slow to converge due to the constraint of stability conditions in the step size τ . In order to speed up the convergence of (4), we may linearize nonlinear 'coefficients' in the associated system and define the iteration step as follows:

$$\begin{cases}
\frac{u_{1}^{[k+1]} - u_{1}^{[k]}}{\tau} - \alpha \nabla \cdot \left(\frac{\nabla u_{1,x}^{[k]}}{\sqrt{(u_{1,x}^{[k]})^{2} + (u_{1,y}^{[k]})^{2} + \beta}} \right) \\
= -f_{1}(\boldsymbol{u}^{[k]}), \\
\frac{u_{2}^{[k+1]} - u_{2}^{[k]}}{\tau} - \alpha \nabla \cdot \left(\frac{\nabla u_{2,x}^{[k+1]}}{\sqrt{(u_{2,x}^{[k]})^{2} + (u_{2,y}^{[k]})^{2} + \beta}} \right) \\
= -f_{2}(\boldsymbol{u}^{[k]})
\end{cases} (5)$$

The idea of the linearized gradient descent (LGD) method in (5) is to linearize and solve the EL equation via a fixed-point (FP) iteration in a similar way to the so-called *Lagged-diffusivity* method¹⁵ or Quasi-Newton scheme. For each iteration, a linear system needs to be solved. As can be seen, both gradient descent

methods in (4) and (5) share two drawbacks. At first, these gradient descent methods provide only the the approximate solutions of the original problem (2), since the TV regularizer $\mathcal{R}(u)$ in (3) is replaced with

$$\mathcal{R}_{\beta}(\boldsymbol{u}) = \sum_{l=1}^{2} \mathcal{R}_{\beta}^{\text{TV}}(u_{l})$$
 (6)

where

$$\mathcal{R}_{\beta}^{\mathrm{TV}}(u_l) = \int_{\Omega} |\nabla u_l|_{\beta} \mathrm{d}\mathbf{x} = \int_{\Omega} \sqrt{u_{l,x}^2 + u_{l,y}^2 + \beta} \mathrm{d}\mathbf{x}$$

is used to avoid non-differentiability of $\mathcal{R}^{TV}(u_l)$ and thus approximated to get (4) and (5). On the second, the choice of β will effect on the computational efficiency of the numerical methods and the smoothness of the constructed deformations. Larger the β , more efficient the methods are, whereas more smooth the condeformations will be. Therefore registration performance in smoothing deformations by these gradient descent methods is very sensitive to the parameter β . Indeed, there are a few different methods existing in the literature for solving the associated EL equation of (2). For example, the use of the nonlinear multigrid (NMG) methods can be found in literature. 5-7,18 However, these existing NMG methods also suffer from difficulties related to the nondifferentiability and non-linearity of $\mathcal{R}^{TV}(u_l)$. To develop efficient numerical methods for TV-based image registration is still a challenging task and has been an active research area so far.

Recently, the variable-splitting methods are the well-known techniques in the field of image restoration for solving variational models, which require the minimization of nonlinear and non-differentiable functionals. To the best of the author's knowledge, the variable-splitting methods for TV-based image registration model in (2) are still missing in the literature. In this paper, the proposed method is based on the so-called augmented Lagrangian method (ALM). We compare the performance of the proposed ALM with the LGD method in (5) and the NMG method developed by literature. Numerical results show that our proposed ALM is more computationally efficient than these existing methods

The rest of this paper is organized as follows. In the second section, we derive our ALM algorithm to solve the variational problem (2), following its numerical implementation in the third section. In the fourth section, numerical comparisons are carried out to confirm the effectiveness of the proposed ALM. Finally, some concluding remarks are made in the last section.

The proposed ALM

Before we derive the proposed ALM, we first rewrite (2) as

$$\min_{\mathbf{u}} \left\{ \mathcal{J}(\mathbf{u}) = \mathcal{D}(\mathbf{u}) + \alpha \sum_{l=1}^{2} \int_{\Omega} |\nabla u_{l}| d\mathbf{x} \right\}$$
(7)

Next, we introduce an auxiliary variable $w = (w_1, w_2)$ such that $w_l = \nabla u_l$ and reformulate the minimization problem (7) to the following constrained minimization problem

$$\min_{\boldsymbol{u},\boldsymbol{w}} \mathcal{J}(\boldsymbol{u},\boldsymbol{w}) \tag{8}$$

$$\mathcal{J}(\boldsymbol{u}, \boldsymbol{w}) = \mathcal{D}(\boldsymbol{u}) + \alpha \sum_{l=1}^{2} \int_{\Omega} |\boldsymbol{w}_{l}| d\mathbf{x}$$

s.t.
$$\mathbf{w}_1 = \nabla u_1$$
 for $1 = 1, 2$

For the minimization of (8), this work proposes to use the ALM and rewrite the constrained minimization problem (8) into an unconstrained minimization problem. We define the augmented Lagrangian functional for the above constrained minimization as follows

$$\mathcal{L}(\boldsymbol{u}, \boldsymbol{w}; \boldsymbol{\lambda}_1, \boldsymbol{\lambda}_2) = \mathcal{J}(\boldsymbol{u}, \boldsymbol{w}) + \sum_{l=1}^{2} \frac{\theta_l}{2} \int_{\Omega} |\boldsymbol{w}_l - \nabla u_l|^2 d\mathbf{x}$$
$$+ \sum_{l=1}^{2} \int_{\Omega} \boldsymbol{\lambda}_l \cdot (\boldsymbol{w}_l - \nabla u_l) d\mathbf{x}$$

where θ_1, θ_2 are the positive penalty parameters and λ_1, λ_2 are the Lagrange multipliers.

Algorithm 1. ALM for TV-based image registration

- 1) Initialization: set m = 0, choose $\theta_1, \theta_2 > 0$ and $\lambda_1^{(0)}, \lambda_2^{(0)}$.
- 2) Repeat
 - 2.1) Compute $(\boldsymbol{u}^{(m)}, \boldsymbol{w}^{(m)})$ as an (approximate) minimizer of the augmented Lagrangian functional with the Lagrange multipliers $\boldsymbol{\lambda}_1^{(m-1)}, \, \boldsymbol{\lambda}_2^{(m-1)}$, i.e.,

$$(\boldsymbol{u}^{(m)}, \boldsymbol{w}^{(m)}) \approx \underset{\boldsymbol{u}, \boldsymbol{w}}{\operatorname{argmin}} \ \mathcal{L}(\boldsymbol{u}, \boldsymbol{w}; \boldsymbol{\lambda}_1^{(m-1)}, \boldsymbol{\lambda}_2^{(m-1)})$$
 (10)

2.2) Update Lagrange multipliers

$$\lambda_1^{(m)} \leftarrow \lambda_1^{(m-1)} + \theta_1(\mathbf{w}_1^{(m)} - \nabla u_1^{(m)})$$
 (11)

$$\lambda_2^{(m)} \leftarrow \lambda_2^{(m-1)} + \theta_2(\mathbf{w}_2^{(m)} - \nabla u_2^{(m)})$$
 (12)

until a stopping rule for ALM method is satisfied.

We propose an iterative algorithm to solve the minimization of $\mathcal{L}(u, w; \lambda_1, \lambda_2)$; see Algorithm 1. Since u and w are coupled together in the minimization problem (9), it is very difficult to solve all variables simultaneously. We separate the minimization problem into two sub-problems and develop an alternating minimization procedure to approximate the solution. This process is repeated until one of the following stopping rules is satisfied:

$$RelSSD^{(m)} = \frac{\mathcal{D}(\boldsymbol{u}^{(m)})}{\mathcal{D}(\boldsymbol{u}^{(0)})} < \epsilon_1, \tag{13}$$

$$\max \left\{ \frac{\|u_1^{(m)} - u_1^{(m-1)}\|}{\|u_1^{(m)}\|}, \frac{\|u_2^{(m)} - u_2^{(m-1)}\|}{\|u_2^{(m)}\|} \right\} < \epsilon_2, \quad (14)$$

$$\max \left\{ \frac{\|\boldsymbol{w}_{1}^{(m)} - \nabla u_{1}^{(m)}\|}{|\Omega|}, \frac{\|\boldsymbol{w}_{2}^{(m)} - \nabla u_{2}^{(m)}\|}{|\Omega|} \right\} < \epsilon_{3}, \quad (15)$$

$$\max \left\{ \frac{\|\boldsymbol{\lambda}_{1}^{(m)} - \boldsymbol{\lambda}_{1}^{(m-1)}\|}{\|\boldsymbol{\lambda}_{1}^{(m)}\|}, \frac{\|\boldsymbol{\lambda}_{2}^{(m)} - \boldsymbol{\lambda}_{2}^{(m-1)}\|}{\|\boldsymbol{\lambda}_{2}^{(m)}\|} \right\} < \epsilon_{4}, \quad (16)$$

$$m \ge \epsilon_5,$$
 (17)

where ϵ_1 , ϵ_2 , ϵ_3 and ϵ_4 denote the predefined small positive numbers, and ϵ_5 is the maximum iteration. Here m denotes the index of the current iteration.

The two-subproblems are as follows: \mathbf{u} -subproblem. Given $\mathbf{w} = (\mathbf{w}_1, \mathbf{w}_2)$, λ_1 and λ_2 , we search a minimizer $\mathbf{u} = (u_1, u_2)^{\top}$ of the minimization problem:

$$\min_{\mathbf{u}} \ \mathcal{J}(\mathbf{u}) \tag{18}$$

$$\mathcal{J}(\boldsymbol{u}) = \mathcal{D}(\boldsymbol{u}) + \sum_{l=1}^{2} \frac{\theta_{l}}{2} \int_{\Omega} |\boldsymbol{w}_{l} - \nabla u_{l}|^{2} d\mathbf{x} - \sum_{l=1}^{2} \int_{\Omega} \nabla u_{l} \cdot \boldsymbol{\lambda}_{l} d\mathbf{x}$$
(19)

According to the calculus of variation, the solution of *u*-subproblem is determined by the associated EL equation

$$\begin{cases} -\theta_1 \triangle u_1 + f_1(\boldsymbol{u}) = g_1, \\ -\theta_2 \triangle u_2 + f_2(\boldsymbol{u}) = g_2, \end{cases}$$
 (20)

subject to the homogeneous Neumann boundary conditions $\frac{\partial u_l}{\partial \mathbf{n}} = 0$, where \mathbf{n} denotes the unit outward

normal vector on the image boundary $\partial \Omega$, $f_l(\boldsymbol{u}) = (T_{\boldsymbol{u}} - R)\partial_{u_l}T_{\boldsymbol{u}}$, $g_l = -\theta_1\nabla\cdot\boldsymbol{w}_l - \nabla\cdot\boldsymbol{\lambda}_l$, and l = 1, 2. **w-subproblem**. Given \boldsymbol{u} , $\boldsymbol{\lambda}_1$ and $\boldsymbol{\lambda}_2$, the following minimization problem

$$\min_{\mathbf{w}} \ \mathcal{J}(\mathbf{w}) \tag{21}$$

$$\mathcal{J}(\mathbf{w}) = \alpha \sum_{l=1}^{2} \int_{\Omega} |\mathbf{w}_{l}| d\mathbf{x} + \sum_{l=1}^{2} \frac{\theta_{l}}{2} \int_{\Omega} |\mathbf{w}_{l} - \nabla u_{l}|^{2} d\mathbf{x}$$
$$+ \sum_{l=1}^{2} \int_{\Omega} \mathbf{w}_{l} \cdot \lambda_{l} d\mathbf{x},$$
(22)

is solved for $w = (w_1, w_2)$. Despite the fact that the variables w_1 and w_2 do not decouple we can still explicitly solve this minimization problem for w using the generalized shrinkage formula as used in:

$$\mathbf{w}_{l} = \max\left(|\mathbf{S}_{l}| - \frac{\alpha}{\theta_{l}}, 0\right) \frac{\mathbf{S}_{l}}{|\mathbf{S}_{l}|}$$
 (23)

with the convection $(\frac{0}{|0|} = 0)$, where $S_l = \nabla u_l - \frac{\lambda_l}{\theta_l}$ and l = 1, 2. Note that several numerical methods, such as iterative reweighted least squares and interior-point method, have been applied to the minimization of subproblems as represented in (21), but these methods cannot usually converge to satisfactory solutions, especially for large-scale problems. To guarantee the convergence of minimization of subproblem (21), as well as to reduce the costs of numerical computation, generalized shrinkage/thresholding functions as given in (23) are employed as the solvers; see literature.

Numerical implementation

In this section, we present the details of how to solve the equation (20) and update the variables w_1 , w_2 , λ_1 , and λ_2 for each iteration.

Finite difference discretization

In order to discretize the EL equation (20), let

$$\left(u_{l}^{h}\right)_{i,j} = u_{l}^{h}(x_{1_{i}}, x_{2_{j}}), \left(\mathbf{u}^{h}\right)_{i,j} = \left(\left(u_{1}^{h}\right)_{i,j}, \left(u_{2}^{h}\right)_{i,j}\right)^{\top}$$

$$(w_{l,1}^h)_{i,j} = w_{l,1}^h(x_{1_i}, x_{2_j}), (w_{l,2}^h)_{i,j} = w_{l,2}^h(x_{1_i}, x_{2_j}),$$

$$\left(\mathbf{w}_{l}^{h}\right)_{i,j} = ((w_{l,1}^{h})_{i,j}, (w_{l,2}^{h})_{i,j}), (g_{l}^{h})_{i,j} = g_{l}^{h}(x_{1_{i}}, x_{2_{j}}),$$

denote the grid functions for l=1, 2 with the grid spacing $h=(h_1,h_2)=(1/n_1,1/n_2)$, where the integers $n_1=1/h_1$ and $n_2=1/h_2$ are the number of uniform intervals in the x_1 and x_2 coordinate directions. Each grid point \mathbf{x} in the discretized domain $\Omega_h \subset \Omega$ is given by $\mathbf{x}=(x_{1_i},x_{2_j})^\top=\left(\frac{(2i-1)h_1}{2},\frac{(2j-1)h_2}{2}\right)^\top$ for $1 \leq i \leq n_1$ and $1 \leq j \leq n_2$.

Applying the finite difference approximations with (20), the discrete EL equation at a grid point (x_{1_i}, x_{2_j}) over the discrete domain Ω_h is given by

$$\begin{cases}
\underbrace{-\theta_{1} \triangle^{h} (u_{1}^{h})_{i,j} + f_{1}^{h} (\boldsymbol{u}^{h})_{i,j}}_{\mathcal{N}_{1}^{h} (\boldsymbol{u}^{h})_{i,j}} = (g_{1}^{h})_{i,j}, \\
\underbrace{-\theta_{2} \triangle^{h} (u_{2}^{h})_{i,j} + f_{2}^{h} (\boldsymbol{u}^{h})_{i,j}}_{\mathcal{N}_{2}^{h} (\boldsymbol{u}^{h})_{i,j}} = (g_{2}^{h})_{i,j},
\end{cases} (24)$$

with the following notation

$$\begin{split} \delta_{x_{1}}^{-}(u_{l}^{h})_{i,j} &= ((u_{l}^{h})_{i,j} - (u_{l}^{h})_{i-1,j})/h_{1}, \\ \delta_{x_{1}}^{+}(u_{l}^{h})_{i,j} &= ((u_{l}^{h})_{i+1,j} - (u_{l}^{h})_{i,j})/h_{1}, \\ \delta_{x_{2}}^{-}(u_{l}^{h})_{i,j} &= ((u_{l}^{h})_{i,j} - (u_{l}^{h})_{i,j-1})/h_{2}, \\ \delta_{x_{2}}^{+}(u_{l}^{h})_{i,j} &= ((u_{l}^{h})_{i,j+1} - (u_{l}^{h})_{i,j})/h_{2}, \\ \nabla^{h}(u_{l}^{h})_{i,j} &= (\delta_{x_{1}}^{+}(u_{l}^{h})_{i,j}, \delta_{x_{2}}^{+}(u_{l}^{h})_{i,j})^{\top}, \\ \nabla^{h} \cdot (\mathbf{w}_{l}^{h})_{i,j} &= \delta_{x_{1}}^{-}(w_{l,1}^{h})_{i,j} + \delta_{x_{2}}^{-}(w_{l,2}^{h})_{i,j}, \\ -\Delta^{h}(u_{l}^{h})_{i,j} &= -\nabla^{h} \cdot (\nabla^{h}(u_{l}^{h})_{i,j}), \\ &= \frac{1}{h_{1}^{2}}((\Sigma)_{i,j}^{h}(u_{l}^{h})_{i,j} - (\bar{\Sigma}^{h})_{i,j}(u_{l}^{h})_{i,j}), \\ (\Sigma)_{i,j}^{h} &= 2(1+\gamma^{2}), \ \gamma = h_{1}/h_{2}, \\ (\bar{\Sigma})_{i,j}^{h}(u_{l}^{h})_{i,j} &= (u_{l}^{h})_{i+1,j} + (u_{l}^{h})_{i-1,j} + \gamma^{2}(u_{l}^{h})_{i,j+1} \\ &+ \gamma^{2}(u_{l}^{h})_{i,j-1}, \\ f_{1}^{h}(\mathbf{u}^{h})_{i,j} &= f_{1}^{h}(u_{1}^{h}, u_{2}^{h})_{i,j} \\ &= (T_{i,j}^{h^{*}} - R_{i,j}^{h}) \frac{T_{i+1,j}^{h^{*}} - T_{i-1,j}^{h^{*}}}{2h_{1}}, \\ f_{2}^{h}(\mathbf{u}^{h})_{i,j} &= f_{2}^{h}(u_{1}^{h}, u_{2}^{h})_{i,j} \end{split}$$

$$= (T_{i,j}^{h^*} - R_{i,j}^h) \frac{(T_{i,j+1}^{h^*} - T_{i,j-1}^{h^*})}{2h_2},$$

$$T_{i,j}^{h^*} = T^h (i + (u_1^h)_{i,j}, j + (u_2^h)_{i,j}),$$

$$(g_l^h)_{i,j} = -\delta_{x_1}^- (\theta_l(w_{l,1}^h)_{i,j} + (\lambda_{l,1}^h)_{i,j})$$

$$-\delta_{x_2}^- (\theta_l(w_{l,2}^h)_{i,j} + (\lambda_{l,2}^h)_{i,j}).$$

We note that all finite difference approximations need to be adjusted at the image boundary $\partial \Omega_h$ using the approximations of the boundary conditions

$$(u_l^h)_{i,1} = (u_l^h)_{i,2}, (u_l^h)_{i,n_2} = (u_l^h)_{i,n_2-1},$$

$$(u_l^h)_{1,i} = (u_l^h)_{2,i}, (u_l^h)_{n_1,i} = (u_l^h)_{n_1-1,i}.$$

In the following subsections the symbols 'h' and ' $(\cdot)_{i,j}$ ' will sometimes drop for simplicity.

Nonlinear multigrid method for solving u-subproblem

The most difficult part of the proposed ALM is the solution of the EL equation for *u*-subproblem in (20). This subproblem is nonlinear and impossible to obtain a closed-form solution. It therefore requires one to approximately solve the corresponding nonlinear discrete system via some iterative method (e.g., a FP method and a Newton-type method). As is well-known, the computational costs of iterative methods are too expensive and we are motivated to develop an efficient numerical method for reducing the computational work.

In this section, we propose a nonlinear multigrid (NMG) method due to literature.²² The basic idea is to accurate the convergence of some basic iterative method on the finest grid by relying on the complementary interplay of smoothing and coarse-grid correction principles. For a more comprehensive treatment of MG methods in the area of image registration, we refer literature^{5,11,18,23–28} and references therein.

Let us denote the nonlinear discrete system in (24) using the following notation:

$$\begin{cases} \mathcal{N}_1^h(\mathbf{u}^h) = g_1^h, \\ \mathcal{N}_2^h(\mathbf{u}^h) = g_2^h \end{cases}$$
 (25)

where u^h denotes the exact solution. Let $\bar{u}^h = (\bar{u}_1^h, \bar{u}_2^h)^{\top}$ be an approximate solution of u^h resulting from applying a few iterations of the smoother on a fine-grid Ω_h (pre-smoothing step). Define the algebraic error as

 $e^h = u^h - \bar{u}^h$. Therefore, the residual equation is given by

$$\mathcal{N}_l^h(\bar{\boldsymbol{u}}^h + \boldsymbol{e}^h) - \mathcal{N}_l^h(\bar{\boldsymbol{u}}^h) = g_l^h - \mathcal{N}_l^h(\bar{\boldsymbol{u}}^h) = r_l^h \, (l = 1, 2).$$

To correct \bar{u}^h numerically on Ω_h , e^h is required to compute, but this computation is considerably and prohibitively expensive on Ω_h . Since the smoother in the pre-smoothing step removes the high frequency component of the error, one can represent the nonlinear system to the coarse grid Ω_H as given by

$$\underbrace{\mathcal{N}_{l}^{h}(\bar{\boldsymbol{u}}^{h} + \boldsymbol{e}^{h})}_{\mathcal{N}_{l}^{h}(\boldsymbol{u}^{h})} = \underbrace{r_{l}^{h} + \mathcal{N}_{l}^{h}(\bar{\boldsymbol{u}}^{h})}_{g_{l}^{h}}$$

$$\downarrow \qquad \qquad \downarrow \qquad \qquad$$

where H is the index for the new cell size $H_1 \times H_2$ with $H_1 \ge h_1$ and $H_2 \ge h_2$. Next, the nonlinear residual equation (27) on Ω_H has to be solved by an efficient method (the coarsest grid solver). The coarse-grid correction $e^H = u^H - \bar{u}^H$ on Ω_H is then interpolated back to that on the fine grid e^h , which can now be used to update \bar{u}^h on Ω_h by using $\bar{u}^h_{new} = \bar{u}^h + e^h$ (coarse-grid correction step). Finally, the smoother is again performed with a few iterations on Ω_h to remove high frequency parts of the interpolated error (post-smoothing step). This procedure is known as a two-grid cycle, and it can be extended to a MG method with recursive application.

Below, we provide the technical details for our MG components.

- 1. The *standard coarsening method* is used in Ω_H by doubling the grid spacing in each space direction i.e. $h_l \rightarrow 2h_l = H_l$ for l = 1, 2.
- 2. The restriction operator I_h^H and interpolation operators I_H^h are used as the intergrid transfer operators and determined by the averaging and bilinear interpolation techniques cf. literature^{29–33} for more details.
- 3. The *discretization coarse grid approximation method* is used to compute the coarse-grid operators.
- 4. The *coarsest grid solver* is the LGD method.
- 5. The MG cycle is $V(\nu_1; \nu_2)$ -cycle, where ν_1 and ν_2 denote respectively the numbers of pre- and post-smoothing steps.
- 6. The MG smoother to be discussed shortly in the next section is obtained from a coupled outer-inner iteration method using a relaxation parameter ω .

The implementation of the proposed NMG method can be summarized as follows: $\bar{u}^h \leftarrow \text{NMGCYC}(\bar{u}^h, g_1^h, g_2^h, R^h, T^h, \nu_1, \nu_2, \theta_1, \theta_2, \omega, \text{Siter})$

1) If $\Omega_h = coarsest\ grid\ (|\Omega_h| = 4 \times 4)$, solve (25) using the LGD method and then stop.

Else continue with following step.

2) Pre-smoothing:

For k = 1 to ν_1 ,

 $[\bar{\boldsymbol{u}}^h] \leftarrow Smoother(\bar{\boldsymbol{u}}^h, g_1^h, g_2^h, R^h, T^h, \theta_1, \theta_2, \omega, Siter)$

(Siter represents the maximum number of the inner iterations)

3) Restriction to the coarse grid:

$$\bar{u}_1^H \leftarrow I_h^H \bar{u}_1^h, \ \bar{u}_2^H \leftarrow I_h^H \bar{u}_2^h, \ R^H \leftarrow I_h^H R^h, \ T^H \leftarrow I_h^H T^h$$

- 4) Set the initial solution for the coarse-grid problem: $\left[\tilde{u}_1^H, \tilde{u}_2^H\right] \leftarrow \left[\bar{u}_1^H, \bar{u}_2^H\right]$
- 5) Compute the new right-hand side for the coarsegrid problem:

$$g_1^H \leftarrow I_h^H(g_1^h - \mathcal{N}_1^h(\bar{\boldsymbol{u}}^h)) + \mathcal{N}_1^H(\bar{\boldsymbol{u}}^H), g_2^H \leftarrow I_h^H(g_2^h - \mathcal{N}_2^h(\bar{\boldsymbol{u}}^h)) + \mathcal{N}_2^H(\bar{\boldsymbol{u}}^H)$$

6) Implement the NMG method on the coarse-grid problem:

$$\bar{\boldsymbol{u}}^H \leftarrow \text{NMGCYC}(\bar{\boldsymbol{u}}^H, g_1^H, g_2^H, R^H, T^H, \nu_1, \nu_2, \theta_1, \theta_2, \omega, \text{Siter})$$

7) Add the coarse-grid corrections:

$$\bar{u}_{1}^{h} \leftarrow \bar{u}_{1}^{h} + I_{H}^{h}(\bar{u}_{1}^{H} - \tilde{u}_{1}^{H}), \ \bar{u}_{2}^{h} \leftarrow \bar{u}_{2}^{h} + I_{H}^{h}(\bar{u}_{2}^{H} - \tilde{u}_{2}^{H})$$

8) Post-smoothing:

For k = 1 to ν_2 ,

$$[\bar{\boldsymbol{u}}^h] \leftarrow Smoother(\bar{\boldsymbol{u}}^h, g_1^h, g_2^h, R^h, T^h, \theta_1, \theta_2, \omega, Siter)$$

To solve *u*-subproblem using (25) numerically, the proposed NMG method is stopped if the maximum number of the MG cycles ε_1 is reached or the mean of the relative residuals obtained from the discrete EL equation (25) is smaller than a small prescribed number $\varepsilon_2 > 0$.

Finally, the pseudo-code implementation of the proposed NMG method can be given in Algorithm 2.

Algorithm 2 The NMG algorithm for *u*-subproblem

$$\bar{\boldsymbol{u}}^h \leftarrow \text{NMG}\Big(\bar{\boldsymbol{u}}^h, g_1^h, g_2^h, R^h, T^h, \nu_1, \nu_2, \theta_1, \theta_2, \omega, \text{Siter}, \vec{\epsilon}\Big)$$

1) Initialization: select $\vec{\varepsilon} = (\varepsilon_1, \varepsilon_2)^{\top}$, set K = 0, $[\bar{\boldsymbol{u}}^h]^{[K]} = \bar{\boldsymbol{u}}^h$ and RelRes $= \varepsilon_2 + 1$.

2) Repeat

2.1)
$$[\bar{\boldsymbol{u}}^h]^{[K+1]} \leftarrow \text{NMGCYC}([\bar{\boldsymbol{u}}^h]^{[K]}, \boldsymbol{g}_1^h, \boldsymbol{g}_2^h, \boldsymbol{R}^h, \boldsymbol{T}^h, \nu_1, \nu_2, \theta_1, \theta_2, \omega, \text{Siter}).$$

2.2) Compute

$$RelRes = mean \left\{ \frac{||\mathbf{g}_{l}^{h} - \mathcal{N}_{l}^{h}([\bar{\mathbf{u}}^{h}]^{[K+1]})||}{||\bar{\mathbf{g}}_{l}^{h} - \mathcal{N}_{l}^{h}([\bar{\mathbf{u}}^{h}]^{[0]})||} \mid l = 1, \dots, 2 \right\}.$$

2.3) Set K = K + 1.

until a stopping rule for NMG method is met.

The MG smoother

Following literature^{5,11,18,23–27} the local Fourier analysis can be used to guarantee that there exists an efficient point-wise smoother within a MG method for solving the discrete nonlinear system (25). To obtain a high-potential point-wise smoother, this work proposes a coupled outer-inner iteration method in a FP framework.

Let ν denote the index for the outer step. We start the outer iteration by introducing the iterative scheme as follows

$$\begin{cases} -\theta_1 \triangle u_1^{[\nu+1]} + f_1(\boldsymbol{u}^{[\nu+1]}) = g_1, \\ -\theta_2 \triangle u_2^{[\nu+1]} + f_2(\boldsymbol{u}^{[\nu+1]}) = g_2. \end{cases}$$

Since this iterative scheme is fully implicit, a linearization procedure of the nonlinear term $f_l(\boldsymbol{u}^{[\nu+1]})$ is required. As pointed out in literature^{5,11,23,26–28} it is appropriate to apply a global linearization technique with the nonlinear terms $f_l(\boldsymbol{u}^{[\nu+1]})$. Thus, the resulting approximation is given by

$$f_{l}(\boldsymbol{u}^{[\nu+1]}) = f_{l}(u_{1}^{[\nu+1]}, u_{2}^{[\nu+1]})$$

$$\approx f_{l}(u_{1}^{[\nu]}, u_{2}^{[\nu]}) + \sigma_{l1}^{[\nu]} \delta u_{1}^{[\nu]} + \sigma_{l2}^{[\nu]} \delta u_{2}^{[\nu]}$$
(27)

where

$$\sigma_{I1}(\boldsymbol{u}^{[\nu]}) = \partial_{u_1} f_I(u_1^{[\nu]}, u_2^{[\nu]})
= (\partial_{u_I} T(\boldsymbol{u}^{[\nu]}))(\partial_{u_1} T(\boldsymbol{u}^{[\nu]}))
+ (T(\boldsymbol{u}^{[\nu]}) - R)(\partial_{u_1 u_I} T(\boldsymbol{u}^{[\nu]})),
\sigma_{I2}(\boldsymbol{u}^{[\nu]}) = \partial_{u_2} f_I(u_1^{[\nu]}, u_2^{[\nu]})
= (\partial_{u_I} T(\boldsymbol{u}^{[\nu]}))(\partial_{u_2} T(\boldsymbol{u}^{[\nu]}))
+ (T(\boldsymbol{u}^{[\nu]}) - R)(\partial_{u_2 u_I} T(\boldsymbol{u}^{[\nu]}))$$

To obtain a simple and fast iterative scheme, we use the approximations for σ_{l1} and σ_{l2} as introduced by literature. ^{11,34–36} Therefore, we have

$$\begin{split} \sigma_{11}(\boldsymbol{u}^{[\nu]}) &= (\partial_{u_1} T_{\boldsymbol{u}^{[\nu]}})(\partial_{u_1} T_{\boldsymbol{u}^{[\nu]}}) \\ &+ (T_{\boldsymbol{u}^{[\nu]}} - R)(\partial_{u_1 u_1} T_{\boldsymbol{u}^{[\nu]}}) \\ &\approx &(\partial_{u_1} T_{\boldsymbol{u}^{[\nu]}})(\partial_{u_1} T_{\boldsymbol{u}^{[\nu]}}), \end{split}$$

$$\begin{split} \sigma_{22}(\boldsymbol{u}^{[\nu]}) &= (\partial_{u_2} T_{\boldsymbol{u}^{[\nu]}}) (\partial_{u_2} T_{\boldsymbol{u}^{[\nu]}}) \\ &+ (T_{\boldsymbol{u}^{[\nu]}} - R) (\partial_{u_2 u_l} T_{\boldsymbol{u}^{[\nu]}}) \\ &\approx (\partial_{u_2} T_{\boldsymbol{u}^{[\nu]}}) (\partial_{u_2} T_{\boldsymbol{u}^{[\nu]}}), \\ \sigma_{12}(\boldsymbol{u}^{[\nu]}) &= \sigma_{21}(\boldsymbol{u}^{[\nu]}) = 0. \end{split}$$

These approximations leads to the following linearized system

$$\begin{cases}
-\theta_{1} \triangle u_{1}^{[\nu+1]} + \sigma_{11}(\boldsymbol{u}^{[\nu]}) u_{1}^{[\nu+1]} = \\
g_{1} - f_{1}(\boldsymbol{u}^{[\nu]}) + \sigma_{11}(\boldsymbol{u}^{[\nu]}) u_{1}^{[\nu]}, \\
-\theta_{2} \triangle u_{2}^{[\nu+1]} + \sigma_{22}(\boldsymbol{u}^{[\nu]}) u_{2}^{[\nu+1]} = \\
g_{2} - f_{2}(\boldsymbol{u}^{[\nu]}) + \sigma_{22}(\boldsymbol{u}^{[\nu]}) u_{2}^{[\nu]}
\end{cases} (28)$$

Next, we apply the finite difference discretization as discussed in Section 3.1 with (28) and solve the associated linear system for each outer step ν by the Gauss-Seidel (GS) method as the inner iteration. The kth step of the GS method defined at a grid point (x_{1_i}, x_{2_j}) is then given by

$$(\mathbf{u}^{[\nu+1]})_{i\,i}^{[k+1]} = (\mathbf{v})_{i\,i}^{[k+1]}$$
 (29)

where

$$\begin{split} (\mathbf{v})_{i,j}^{[k+1]} &= \begin{pmatrix} F_1^{[\nu]} \\ F_2^{[\nu]} \end{pmatrix}, \\ F_1^{[\nu]} &= \begin{pmatrix} \frac{1}{(\theta_1/h_1^2)(\Sigma)_{i,j} + (\sigma_{11}(\mathbf{u}^{[\nu]}))_{i,j}} \end{pmatrix} \\ &\times \left[(g_1)_{i,j} - f_1(\mathbf{u}^{[\nu]})_{i,j} + (\sigma_{11}(\mathbf{u}^{[\nu]}))_{i,j}(\mathbf{u}_1^{[\nu]})_{i,j} \\ &+ (\theta_1/h_1^2)(\bar{\Sigma})_{i,j}(\mathbf{u}_1^{[\nu+1]})_{i,j}^{[k+1/2]} \right] \\ F_2^{[\nu]} &= \begin{pmatrix} \frac{1}{(\theta_2/h_1^2)(\Sigma)_{i,j} + (\sigma_{22}(\mathbf{u}^{[\nu]}))_{i,j}} \end{pmatrix} \times \\ &= \left[(g_2)_{i,j} - f_2(\mathbf{u}^{[\nu]})_{i,j} + (\sigma_{22}(\mathbf{u}^{[\nu]}))_{i,j}(\mathbf{u}_2^{[\nu]})_{i,j} \\ &+ (\theta_2/h_1^2)(\bar{\Sigma})_{i,j}(\mathbf{u}_2^{[\nu+1]})_{i,j}^{[k+1/2]} \right] \end{split}$$

and

$$(\bar{\Sigma})_{i,j}(u_l^{[\nu+1]})_{i,j}^{[k+1/2]} = (u_l^{[\nu+1]})_{i+1,j}^{[k]} + (u_l^{[\nu+1]})_{i-1,j}^{[k+1]}$$

$$+ \gamma^{2} (u_{l}^{[\nu+1]})_{i,j+1}^{[k]}$$
$$+ \gamma^{2} (u_{l}^{[\nu+1]})_{i,j-1}^{[k+1]}$$

Here the superscripts k, k + 1/2, and k + 1 denote the current, intermediate and new approximations computed by the GS method.

In order to obtain more efficiency, one introduces a relaxation parameter $\omega \in (0,2)$ and iterates the successive over relaxation (SOR) steps by

$$(\boldsymbol{u}^{[\nu+1]})_{i,j}^{[k+1]} = (1-\omega)(\boldsymbol{u}^{[\nu+1]})_{i,j}^{[k]} + \omega(\boldsymbol{v})_{i,j}^{[k+1]}$$
(30)

Finally, the implementation of the proposed MG smoother (30) on Ω_h is summarized in Algorithm 3.

Algorithm 3 The MG smoother for the proposed NMG algorithm (Algorithm 2)

$$\bar{\boldsymbol{u}}^h \leftarrow Smoother(\bar{\boldsymbol{u}}^h, g_1^h, g_2^h, R^h, T^h, \theta_1, \theta_2, \omega, Siter)$$

- 1)] Use input parameters to compute $(v)_{i,i}$ for all $1 \le i \le n_1 \text{ and } 1 \le j \le n_2.$
- 2)] Perform SOR steps for k = 0, 1, 2, ..., Siter 2.1)] Update $(\bar{u}^h)_{i,j}^{[k+1]}$ by (30) for all $1 \le i \le n_1$ and $1 \leq j \leq n_2$.

Note that we applied the so-called local Fourier analysis (LFA) to test the smoothing performance of the proposed MG smoother with different values of ω (the relaxation parameter) and Siter (the maximum number of inner iterations) for the four representative registration problems given by Problems 1–4 (as shown respectively in Figure 1. Our results shows that the proposed FP smoother with $\omega = 1.85$ and Siter = 2 is recommended; see its performance in leading the proposed ALM method to fast convergence from Tables 3 and 4. The theoretical details for applying LFA to analyze the proposed smoother are straightforward and similar to our previous work in (11)

The closed form expressions for w_1 , w_2 , λ_1 , and λ_2 Based on the formulation (23), we can get the closed form expressions for w_1 and w_2 as given by

$$(\mathbf{w}_l)_{i,j} = \max\left(\left| (\mathbf{S}_l)_{i,j} \right| - \frac{\alpha}{\theta_l}, 0\right) \frac{(\mathbf{S}_l)_{i,j}}{\left| (\mathbf{S}_l)_{i,j} \right|}, \tag{31}$$

where
$$S_l = \left(\delta_{x_1}^+(u_l)_{i,j} - \frac{(\lambda_{l,1})_{i,j}}{\theta_l}, \delta_{x_2}^+(u_l)_{i,j} - \frac{(\lambda_{l,2})_{i,j}}{\theta_l}\right)^{\top}$$
 for $l=1,2.$

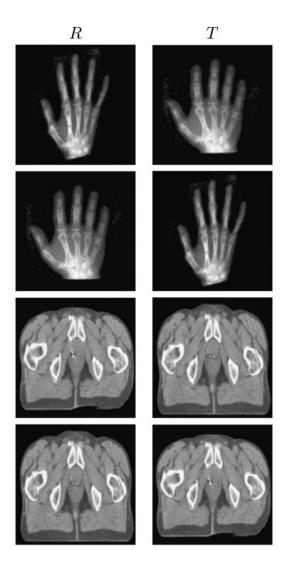


Figure 1. Four registration problems of the real medical images. (left column) Reference images; (right column) Template images; (top row) Problem 1; (2nd row) Problem 2; (3rd row) Problem 3; (bottom row) Problem 4.

Similarly, based on the formulations in (11) and (12), we may update all the Lagrangian multipliers by

$$(\boldsymbol{\lambda}_{1}^{(k+1)})_{i,j} = (\boldsymbol{\lambda}_{1}^{(k)})_{i,j} + \theta_{1}((\boldsymbol{w}_{1})_{i,j}^{(k+1)} - \nabla^{+}(u_{1})_{i,j}^{(k+1)})$$
(32)

$$(\lambda_2^{(k+1)})_{i,j} = (\lambda_2^{(k)})_{i,j} + \theta_2((\mathbf{w}_2)_{i,j}^{(k+1)} - \nabla^+(u_2)_{i,j}^{(k+1)})$$
(33)

Numerical experiments

In this section, we present a number of numerical experiments to

are the LGD method (5) and the NMG method by Chumchob (5)

 assess the accuracy and efficiency of the proposed ALM with regard to parameter changes.

We note first that four registration problems consisting of four real medical images to be denoted as Problems 1–4 were selected for the experiments, as shown respectively in Figure 1. Second, we used $n_1 = n_2 = n$ (i.e. we assume the grid spacing $h_1 = h_2 = h = 1/n$) in all numerical tests. Third, the bilinear interpolation was employed to compute the transformed template image T_u once the deformations are found in all cases. We also note that all numerical algorithms for the proposed ALM, LGD and NMG methods were started with $u^{[0]} = 0$ and implemented under MATLAB R2018a and run on a machine configured with Intel(R) Core(TM) i7 Quad-core 4.2 GHz and 32GB of RAM.

Performance comparison with the other two methods

In this test, the performance of three different methods for TV-based image registration model is compared. We apply the relative SSD (a qualitative measure in the accuracy), time per iteration (in seconds), total CPU time (in seconds), and total iterations to perform our evaluation on the four registration problems shown in Figure 1.

For the LGD method, we chose $\tau = 10^{-5}$ and $\beta = 10^{-6}$ and implemented a direct solver using MATLAB's \-operator (also known as mldivide operator) for solving each linear system of equations arising from applying the FP method with the nonlinear discrete EL system.

For the NMG method, we implemented with the FAS-NMG method of Chumchob (5) The details of our numerical implementation can be summarized as follows. We solved the nonlinear discrete EL system with $\beta=10^{-6}$ in a V-cycle framework, where the coarsest grid is 4×4 . The LGD method was used to solve the coarsest problem with $\tau=10^{-3}$. We used the standard coarsening method and standard interpolation technique for transferring data between grids. We applied 15 pre- and 15 post-smoothing steps with a so-called FP-SOR smoother.

For the proposed ALM, we chose the penalty parameters $\theta_1 = \theta_2 = 1/10$. We used the predefined numbers $\epsilon_1 = 10^{-2}$, $\epsilon_2 = 10^{-4}$, $\epsilon_3 = \epsilon_4 = 10^{-8}$ and $\epsilon_5 = 200$ with Algorithm 1. The predefined numbers $\epsilon_1 = 20$ and $\epsilon_2 = 10^{-6}$ were applied by the proposed NMG method in Algorithm 2 to solve *u*-subproblem. In all registration problems, the proposed NMG method with the MG smoother in Algorithm 3 was performed with the MG parameters, $\nu_1 = \nu_2 = 5$ (5 pre- and 5

post-smoothing steps), $\omega = 1.85$ (the relaxation parameter), and Siter = 2 (2 iterations of SOR steps).

All numerical methods in this test used the same regularization parameter $\alpha = 1/50$ with the grid spacing h = 1/256. Each method was stopped when the

$$\text{relative solution, } \max \left\{ \frac{\|u_1^{(m)} - u_1^{(m-1)}\|}{\|u_1^{(m)}\|}, \frac{\|u_2^{(m)} - u_2^{(m-1)}\|}{\|u_2^{(m)}\|} \right\}, \quad \text{was}$$

brought below 10^{-4} or the number of iterations increases beyond a predefined number. Here we used the predefined numbers $m_{\rm max}^{\rm LGD}=200$ for the LGD method, $m_{\rm max}^{\rm NMG}=50$ for the NMG method, and $m_{\rm max}^{\rm ALM}=200$ for the proposed ALM.

From Table 1, one can see that only the proposed ALM converges, whereas the LGD and NMG methods are unable to converge in a reasonable number of iterations. As expected, we have found in this case that the small value of β has a significant effect on the accuracy of the registered images and the convergence of the LGD and NMG method. Moreover, Figure 2 shows that for each registration problem the proposed ALM yields the best value of the relative SSD. It is important to note that the smaller the value of the relative SSD is, the accurate registered image is achieved. This evidence ensures that the registration results by the proposed ALM are more reliable than the LGD and NMG methods. Particularly, Figure 3 shows that the proposed ALM is computationally efficient than the other two methods in delivering the high quality of the registered images. The proposed ALM takes only a few iterations (say 5 iterations) to drop the relative SSD below 0.20, which means that the dissimilarities between the reference and registered images have been reduced more than 80% within the first 5 iterations. This is a remarkable result to conclude that the computational performance of the proposed ALM in solving TVbased image registration is much more efficient than those of the other two methods.

In terms of computation times per iteration, we can see that the proposed ALM requires to solve two subproblems for u and w in each step. Thus, in accordance with our measurements, we expect that more computation time per iteration is required for the proposed ALM than those of the other two methods. As can be seen from Table 1, our numerical experiments reflect this expectation.

In terms of total CPU times, Table 1 illustrates the LGD method is the slowest method, while the NMG method is slightly faster than the proposed ALM. However, both LGD and NMG method are unable to converge. Thus we can conclude that the LGD and NMG methods are less computationally efficient than the proposed ALM.

In Figure 4 we present the constructed deformations by the proposed ALM for all registration problems.

Table I. Comparison of the relative SSD, time per iteration, total CPU time (s), and total iterations by three different numerical methods on the four registration problems in Figure I with $\alpha = \frac{1}{50}$ and $h = \frac{1}{256}$. * indicates that maximum number of iterations reached without convergence.

Method	Registration problem				
	I	2	3	4	
LGD					
Relative SSD	0.8027	0.7853	0.7841	0.8250	
Time per iteration (s)	0.2467	0.2458	0.2457	0.2463	
Total CPU time (s)	49.3423	49.1558	49.1301	49.2524	
Total iterations	200*	200*	200*	200*	
NMG					
Relative SSD	0.2465	0.1670	0.0710	0.0852	
Time per iteration (s)	0.4941	0.4930	0.4814	0.4914	
Total CPU time (s)	24.7045	24.6477	24.0701	24.5724	
Total iterations	50*	50*	50*	50 *	
Proposed ALM					
Relative SSD	0.1836	0.1476	0.0664	0.0681	
Time per iteration (s)	0.5970	0.6893	0.7105	0.7138	
Total CPU time (s)	28.4776	40.6674	37.6567	38.5466	
Total iterations	41	59	53	54	

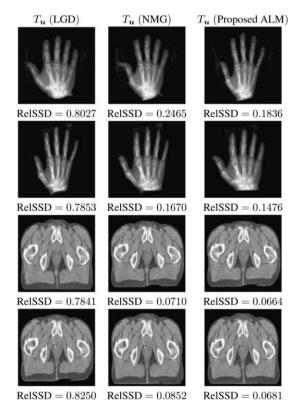


Figure 2. Qualitative comparison of registered images by three different methods on the four registration problems in Figure 1. (*left*) Registered images by LGD; (*middle*) registered images by NMG; (*right*) registered images by the proposed ALM. 'ReISSD' means the relative SSD defined in (13) to represent the dissimilarities between R and T_u . Note that the small the value of ReISSD is, the accurate registered image is obtained.

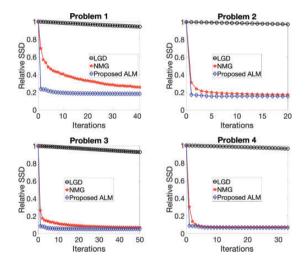


Figure 3. History of the relative SSD by three different methods in solving the four registration problems in Figure 1.

In Figure 5, we show the constructed surfaces of both components of the deformations in Figure 4. In Figure 6, we present the middle slices of the constructed surfaces of the components of the deformations in Figure 5. As expected from the use of TV regularizer, the visual inspection in Figure 4 shows that the proposed ALM delivers the visually appealing results in preserving the discontinuities of the constructed deformation as shown in the corresponding close-up regions. We can also see in Figure 4 that the constructed deformation yields multiple motions in the image to be registered and the motion discontinuities can be observed at the boundaries of the local

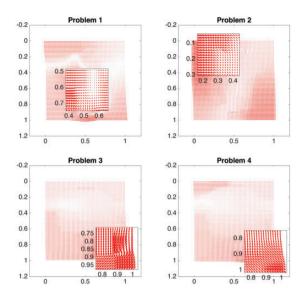


Figure 4. Constructed deformations by the proposed ALM for the four registration problems in Figure 1. Note that multiple motions in the corresponding image and motion discontinuities at the boundaries of the local regions determined by the constructed deformation can be observed in the corresponding close-up regions.

regions. We see further that the corresponding deformation in each registration problem is neither smooth nor reflecting a homogeneous motion. For each local region, the motion tends to change smoothly, and the gradients of the constructed deformation in this area are small. At the boundaries of the local regions, the gradients of the constructed deformation are large, and the discontinuities of the constructed deformation can be observed. Moreover, we can see from Figures 5 and 6 that the constructed surfaces of both components of the deformations are non-smooth and their middle slices are almost piecewise constant for all registration problems.

To summarize we have successfully developed the efficient and effective numerical method for TV-based image registration model. Our registration results on the real medical applications shown in Figure 1 demonstrate that the proposed ALM is more computationally efficient and effective than the other two methods. The most attractive features of our proposed method is that it is able to produce the high quality of the registered images in a reasonable number of iterations while it satisfies the requirement in constructing the deformations by the TV regularizer.

Performance tests with the regard to parameter changes

We now present numerical results from several test cases, to assess the accuracy and efficiency of our proposed numerical techniques with the regard to parameter changes.

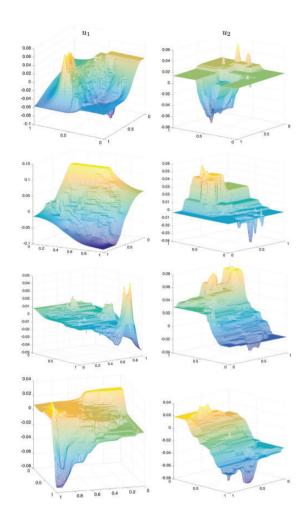


Figure 5. Constructed surfaces of both components of the constructed deformations by the proposed ALM for the four registration problems in Figure 1. (*left*) the first component u_1 ; (*right*) the second component u_2 ; (*top row*) Problem 1; (*2nd row*) Problem 2; (*3rd row*) Problem 3; (*bottom row*) Problem 4.

h-Independence test. One of the key properties of MG techniques is that their convergence does not depend on the number of grid points. Thus, in this test we designed our numerical experiments to investigate this property with the proposed ALM in Algorithm 1, and to back up our proposed NMG method in Algorithms 2.

We implemented the proposed ALM with the same regularization parameter $\alpha = \frac{1}{250}$ and the penalty parameters θ_1 and θ_2 as shown in Table 2. In order to stop our proposed ALM, we used the same predefined numbers used in Section 4.1. We also used the same MG parameters to solve *u*-subproblem as given in the previous section.

In the numerical results shown in Table 2, one can see five quantities: the relative SSD, the total iterations, the total CPU times (in seconds), the ratio of the total CPU times in increasing both image dimensions by a factor of 2, and the number of average MG steps used to solve u-subproblem by Algorithm 2 with different values of grid spacing h.

As expected from a numerical technique using a MG framework, Table 2 shows that Algorithm 1 not only

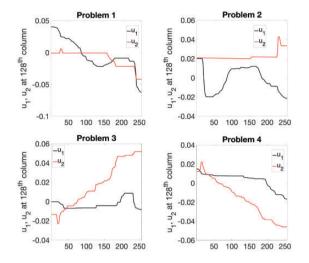


Figure 6. The middle slices of the corresponding surfaces of both components of the constructed deformations shown in Figure 5 by the proposed ALM.

converges within a few iterations, but it also provides the accurate registration results because the dissimilarities between the reference and registered images given have been reduced more than 90% for Problem 1, 89% for Problem 2, and 96% for Problems 3 and 4. Moreover, the NMG method in Algorithm 2 can reduce the mean of the relative residuals to $\varepsilon_2 = 10^{-6}$ within a few MG steps for different values of h. In addition, we see an increase in the total CPU time by a factor of approximately 4.5 when both image dimensions is increased by a factor of 2. This shows that the proposed ALM has an optimal efficiency resulting from the NMG method proposed in Algorithm 2, which should be of order $\mathcal{O}(N\log(N))$ where $N=n^2$. Then we can conclude that the proposed ALM has no effect on the convergence for different values of h.

 α -Dependence test. Next we evaluate to show how our proposed ALM in Algorithm 1 is affected with varying the regularization parameter α .

To this end, we performed the proposed ALM on the four registration problems in Figure 1 with the same grid spacing $h = \frac{1}{256}$ and the penalty parameters θ_1 and θ_2 as given in Table 2. Our proposed ALM in

Table 2. Registration results for Problems I–4 in Figure I by the proposed ALM in Algorithm I with $\alpha = \frac{1}{250}$ and different values of grid spacing h. Note that 'Ratio' means the ratio of the total CPU times in increasing both image dimensions by a factor of 2.

Registration problem	Grid spacing (h)				
	<u>l</u> 256	<u> </u> 512	<u> </u> 1024	<u> </u> 2048	
$\frac{1}{1}(\theta_1 = \theta_2 = 1)$				_	
Relative SSD	0.0968	0.0958	0.0951	0.0951	
Total iterations	22	22	21	21	
Total CPU time (s)	22.4489	74.1501	308.4895	1,308.3476	
Ratio	_	3.3031	4.1603	4.2411	
Average MG cycles	6	6	6	6	
$2 (\theta_1 = \theta_2 = 1)$					
Relative SSD	0.1028	0.1027	0.1025	0.1002	
Total iterations	16	16	15	15	
Total CPU time (s)	16.1900	58.8500	257.0531	1,117.0938	
Ratio	_	3.6350	4.3679	4.4294	
Average MG cycles	7	7	7	7	
$3 (\theta_1 = \theta_2 = \frac{1}{4})$					
Relative SSD	0.0359	0.0359	0.0358	0.0357	
Total iterations	36	34	33	33	
Total CPU time (s)	38.8623	137.9971	577.3338	2,578.2640	
Ratio	_	3.5509	4.1837	4.4658	
Average MG cycles	7	7	7	7	
4 $(\theta_1 = \theta_2 = \frac{1}{4})$					
Relative SSD	0.0377	0.0375	0.0374	0.0373	
Total iterations	31	31	30	30	
Total CPU time (s)	30.9928	116.8559	500.9036	2, 238.7849	
Ratio	_	3.7704	4.2865	4.4695	
Average MG cycles	6	6	6	6	

Table 3. Registration results for Problems I–4 in Figure I by the proposed ALM in Algorithm I with $h=\frac{1}{256}$ and different values of the regularization parameter α

Registration problem	Regularizatio	Regularization parameter (α)					
	<u>l</u> 250	<u>l</u> 200	<u> </u> 150	100	<u>l</u> 50	<u> </u> 25	
$\frac{1}{1}(\theta_1 = \theta_2 = 1)$							
Relative SSD	0.0968	0.1015	0.1080	0.1313	0.2099	0.3466	
Total iterations	20	21	25	30	33	49	
Average MG cycles	6	6	6	6	6	6	
$2 (\theta_1 = \theta_2 = 1)$							
Relative SSD	0.1028	0.1028	0.1069	0.1174	0.1675	0.2104	
Total iterations	16	18	20	27	37	40	
Average MG cycles	7	6	6	6	6	6	
$3 (\theta_1 = \theta_2 = \frac{1}{4})$							
Relative SSD	0.0359	0.0385	0.0436	0.0536	0.0958	0.2251	
Total iterations	36	44	49	65	90	125	
Average MG cycles	7	7	6	6	5	5	
$4 (\theta_1 = \theta_2 = \frac{1}{4})$							
Relative SSD	0.0377	0.0406	0.0449	0.0548	0.0863	0.1909	
Total iterations	31	34	49	57	102	139	
Average MG cycles	6	6	5	5	5	5	

Table 4. Registration results for Problems I-4 in Figure I by the proposed ALM in Algorithm I with $h=\frac{1}{256},~\alpha=\frac{1}{250}$ and different values of the penalty parameter θ . Recall that * indicates that maximum number of MG cycles reached without convergence.

Penalty parameter	Registration problem				
	I	2	3	4	
$\theta = 10$					
Relative SSD	0.8128	0.8128	0.4923	0.5056	
Total iterations	3	3	3	3	
Average MG cycles	20*	15	18	18	
$\theta = 8$					
Relative SSD	0.7721	0.7774	0.4271	0.4401	
Total iterations	3	3	3	3	
Average MG cycles	20*	19	15	15	
$\theta = 6$					
Relative SSD	0.7098	0.7138	0.3476	0.3595	
Total iterations	3	3	3	3	
Average MG cycles	20*	20*	14	14	
$\theta = 4$					
Relative SSD	0.6033	0.6029	0.2615	0.2710	
Total iterations	3	3	3	3	
Average MG cycles	20*	20*	19	19	
$\theta = 2$					
Relative SSD	0.1935	0.2048	0.2187	0.2467	
Total iterations	8	7	10	9	
Average MG cycles	12	14	20*	20*	
$\theta = 1$					
Relative SSD	0.0968	0.1028	0.2057	0.2443	
Total iterations	20	16	17	19	
Average MG cycles	6	7	20*	20*	
$\theta = \frac{1}{2}$					
Relative SSD	0.0693	0.0696	0.0670	0.0441	
Total iterations	39	31	25	19	
Average MG cycles	5	5	20*	20*	

(continued)

Table 4. Continued.

Penalty parameter	Registration problem				
	I	2	3	4	
$\theta = \frac{1}{4}$					
Relative SSD	0.0617	0.0586	0.0359	0.0377	
Total iterations	60	44	36	31	
Average MG cycles	4	5	7	6	
$\theta = \frac{1}{6}$					
Relative SSD	0.0600	0.0549	0.0338	0.0348	
Total iterations	75	60	46	52	
Average MG cycles	4	4	5	5	
$\theta = \frac{1}{8}$					
Relative SSD	0.0584	0.0536	0.0328	0.0340	
Total iterations	89	100	63	59	
Average MG cycles	4	4	5	4	
$\theta = \frac{1}{10}$					
Relative SSD	0.0579	0.0535	0.0326	0.0336	
Total iterations	108	191	75	62	
Average MG cycles	4	4	4	4	

Algorithm 1 was stopped with the same predefined numbers used in Section 4.1. We also applied the same predefined number and MG parameters as shown in Section 4.1 with Algorithms 2 and 3 to solve *u*-subproblem.

Table 3 presents the numerical results by the proposed ALM in Algorithm 1 with different values of the regularization parameter α . It contains three quantities: the relative SSD, the total iterations, and the number of average MG steps used to solve u-subproblem by Algorithm 2.

As presented in Table 3, decreasing the values of α has significant effects on the accuracy of the registered images and the convergence of the proposed ALM in Algorithm 1, whereas the value of α has only a small effect on the convergence of the proposed NMG method in Algorithm 2. We can see that large α is not needed as small ones give better registration results, typically $\alpha = \frac{1}{250}, \frac{1}{200}, \frac{1}{150},$ and $\frac{1}{100}$. It is important to note that the process to select the optimal value of α is a separate but important issue because it is in general unknown a priori and it significantly affects on the accuracy of registered images and the ALM performance.

In order to find a suitable α automatically, the 'cooling' ('continuation') process suggested in literature^{11,35,37–39} is recommended for real applications. The basic idea is to start with a high initial value of α and then slowly reduce α such that the obtained solution can be used to be an excellent starting point for the next in order to decrease \mathcal{J} in (8).

 (θ_1, θ_2) -dependence test. We now present numerical results from several test cases to evaluate the

registration performance of our proposed ALM with different values of θ_1 and θ_2 .

We performed the proposed ALM in Algorithm 1 on the four registration problems shown in Figure 1 using $h = \frac{1}{256}$ and $\alpha = \frac{1}{250}$. The predefined numbers and the MG parameters for Algorithms 1–3 are the same values used in Section 4.1.

We note that we take $\theta_1 = \theta_2 = \theta$ in this numerical test to evaluate the performance of the proposed ALM. Table 4 presents the registration results for the four registration problems by the proposed ALM in Algorithm 1 with different values of θ . Three qualities for the performance tests are the relative SSD, the total iterations, and the number of average MG steps used to solve u-subproblem by Algorithm 2.

One sees from Table 4 that as θ is decreased from 10 to $\frac{1}{10}$ the dissimilarities between the given images decrease (the accuracy of the registered image increase), whereas the cost of the proposed ALM increases. We observe that the smaller θ is the better the proposed NMG method performs and an increase in the number of smoothing steps is required to achieve fast MG convergence for large θ . Next, we see that decreasing the value of θ leads to the best registration result at $\theta = \frac{1}{10}$. We see further that large values of θ are not required as small ones deliver better registration performance. Typically, θ should be between $\frac{1}{10}$ and $\frac{1}{2}$ to give the accurate registration results in a reasonable number of iterations.

Concluding remarks

In this paper, we first explained how standard methods solve the TV-based image registration model. Next, we

discussed how we are needed to develop a new method. In order to efficiently solve the model, we therefore proposed to use augmented Lagrangian method. We separated the associated minimization problem into two subproblems. As a result, the first subproblem is a nonlinear problem and impossible to obtain exact solution, whereas the other one has a closed-form solution. Next, we developed an efficient NMG method to solve the associated discrete nonlinear system. In order to assess the efficiency and effectiveness of our new method, we tested, using four registration problems of real medical images, how our new method performs. We found in our first numerical test that the registered images by different methods are not identical. Therefore, it can be concluded that different numerical algorithms for TV-based image registration model have a significant effect on the accuracy of registered images. We also found that our new method outperforms the existing methods. Moreover we found by the performance comparison in this test that our new method is able to deliver the accurate registration results with the desired properties of the constructed deformations in a reasonable number of iterations. Next, we found in the second test that there are no effect on the convergence of the new method for different numbers of grid points. Moreover, we observed from the third and last tests that the choice of the regularization and penalty parameters is important for the quality of the registered images and the computational performance of the new method. The outlines in selecting these two parameters to obtain the accurate registration results were discussed. Future work will extend the proposed method to high-order variational models for image registration.

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