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405 nm LIGHT EXPOSURE OF OSTEOBLASTS AND INACTIVATION OF BACTERIAL ISOLATES FROM ARTHROPLASTY PATIENTS: POTENTIAL FOR NEW DISINFECTION APPLICATIONS?

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405 nm light exposure of osteoblasts and bacteria

Introduction

Healthcare associated infections (HAI), defined as infections which are not present at the time the patient enters hospital, are an ever increasing problem in modern healthcare affecting approximately 1 in 10 patients admitted to UK hospitals (Reilly et al., 2007). Despite current attempts to resolve the problem, including campaigns to improve hygiene in hospitals, particularly hand washing, HAI still causes significant patient mortality. A report published by the House of Commons in 2004 found that HAIs are responsible for over 5,000 deaths in the UK each year, and are a contributory factor in over 1,500 deaths (National Audit Office, 2004). In the USA, deaths associated with HAI in hospitals exceeded the number attributable to several of the top ten leading causes of death. A survey performed in 2002 found 1.7 million patients with an HAI, of which 155,668 died (Klevens et al., 2007). The rise in prevalence of HAI can partly be attributed to the increased use of antibiotics leading to antibiotic resistant strains of many bacteria (McGowan, 1983). It is clear that novel approaches to bacterial inactivation are required.

HAIs take many forms. The most common type of infection reported by the Scottish National HAI Prevalence Survey was found to be urinary tract infection (UTI), accounting for 17.9 % of cases (Reilly et al., 2008), with a major risk factor being the use of indwelling catheters. Surgical site infections (SSI) are the next most common, accounting for 16 %. The use of indwelling or implanted medical devices is increasing with technological advances, and so the incidence of device-related infection is increasing (von Eiff et al., 2005). Taking infection acquired during hip replacement surgery as a specific example of HAI, studies have shown incidence rates from 1-5 %, increasing considerably after revision procedures (Ridgeway et al., 2005; Hamilton and Jamieson, 2008; Wilson et al., 2008). During mandatory surveillance of 22,160 hip replacement procedures taking place in England between April 2004 and March 2005, Staphylococcus aureus was identified in 64 % of infections, 67 % of which were methicillin-resistant strains (Wilson et al., 2008). Staphylococcus epidermidis has also been identified in a large number of cases (Hamilton and Jamieson, 2008). The source of these infections is many-fold. Patient skin will contribute, but general contamination of the operation site and equipment is a
major issue. This is particularly well documented in a paper by Davis and co-workers from Manchester, UK, reporting that 63 % of operations showed contamination of the field of operation (Davis et al., 1991). A reduction in the bacterial load will therefore be beneficial. Laminar flow ventilation, by which a continuous flow of highly filtered bacteria-free air is recirculated under positive pressure into the operating field and air contaminants generated during surgery are removed from the site, was introduced to orthopaedic operating theatres in the 1980s. However, even with modern laminar flow ventilation, unacceptably high numbers of bacterial isolates are still reported during orthopaedic surgery (Owers et al., 2004), and at the British Hip Society meeting in 2011 McGovern and colleagues demonstrated how easily laminar air flow can be significantly disrupted by external forces during orthopaedic surgery (McGovern et al., 2011). Ultraviolet (UV) light in the operating theatres is more effective than laminar flow ventilation at reducing the number of airborne bacteria, and Ritter et al. (2007) reported that UV radiation reduced the risk of infection in joint replacement procedures from 1.77 to 0.57 %. Despite this effect, UV radiation has not been widely used in the UK as the protective clothing required by operating staff is deemed to be too hot, thick and uncomfortable for routine use (Godsen et al., 1998).

High-intensity narrow-spectrum (HINS) light is a new disinfection method that utilises the phototoxic effect of 405 nm visible blue light without the need for additional photosensitiser molecules (Anderson et al., 2006; Anderson et al., 2007). Although not as bactericidal as UV light, 405 nm light has advantages including increased human safety due to its lower photon energy (Blatchley and Peel, 1991). Previous studies have demonstrated that this 405 nm blue light can inactivate various bacteria, including Staphylococcus aureus, methicillin-resistant S. aureus (MRSA), S. epidermidis and Escherichia coli (Guffey and Wilborn, 2006; Maclean et al., 2008a; Maclean et al., 2009). The mechanism of bacterial inactivation is thought to be by photostimulation of endogenous intracellular porphyrins, which leads to the generation of reactive oxygen species (ROS) (Orenstein et al., 1997; Papageorgiou et al., 2000; Guffey and Wilborn, 2006; Maclean et al., 2008b). Exposure to 405 nm light at doses that inactivate S. epidermidis has been shown to not affect the viability of fibroblasts in vitro, or their contractile activity in a wound healing model – the fibroblast populated collagen hydrogel lattice (McDonald et al., 2011).

The use of 405 nm HINS-light for environmental disinfection has undergone clinical evaluation in occupied patient isolation rooms in Glasgow Royal Infirmery, where it was used as a background lighting system to provide continuous disinfection of air and exposed surfaces in the presence of patients and staff. The results demonstrated a significantly greater reduction in levels of environmental contamination than was achievable by normal disinfection methods alone (Maclean et al., 2010). It is proposed that 405 nm HINS-light has considerable potential to reduce the environmental airborne bacterial load in orthopaedic operating theatres, and decrease the risk of post-operative infection following arthroplasty procedures. To assess the efficacy of 405 nm HINS-light for this application, the susceptibility of bacterial isolates from clinical cases of surgical site infections from arthroplasty procedures to HINS-light was assessed. To ensure in principle that any exposed patient bone tissue would not be detrimentally affected by exposure to lethal doses of 405 nm HINS-light, the effect of exposure of osteoblasts in vitro to bactericidal doses of HINS-light was determined in terms of viability, morphology and function. Osteoblast functions were assessed by alkaline phosphatase (ALP) activity, collagen synthesis and osteocalcin expression.

Materials and Methods

Culture and 405 nm light exposure of osteoblasts
The effect of 405 nm HINS-light was determined on immortalised neonatal rat calvarial osteoblasts cultured in Dulbecco’s Modified Eagle’s Medium (DMEM) supplemented with 10 % v/v foetal calf serum, 1 % v/v non-essential amino acids, penicillin (50 units/mL) and streptomycin (50 μg/mL). Cells were routinely cultured as monolayers in 75 cm² tissue culture flasks in a humidified atmosphere of 5 % CO₂ in air at 37 °C. For experimental use, the required cell concentration was prepared in complete DMEM and seeded onto the surface of multiwell plates (0.2 mL for 96-well plates; 1 mL for 24-well plates), with the seeding density used (5×10⁴ cells/cm² or 2×10⁴ cells/cm²) determined by the post-exposure test being performed. After seeding, cells were incubated for a minimum of 4 h to allow attachment, and then the culture medium was replaced with Dulbecco’s phosphate buffered saline (PBS) for 405 nm HINS-light exposure.

The HINS-light system consisted of a bank of nine narrow-band LEDs (GE Lumination, Cleveland, OH, USA), with peak output at 405 nm and a 20 nm bandwidth at full-width half-maximum, attached to a heat sink supported by two pillars above a moulded base which centralises the position of the treatment dish. The distance between the sample and the LEDs was 8 cm. This short distance was chosen to optimise chances of seeing any deleterious effects of the HINS-light exposure in the experimental setup. The heat sink ensured that the operating temperatures remained constant for the duration of the light treatments, and no heating of samples occurred. Cells were exposed to 1 h durations of 405 nm light with irradiance levels of 0.5, 1.8, 5 and 15 mW/cm², corresponding to doses of 1.8, 6.5, 18 and 54 J/cm². Control cells that were not exposed to HINS-light were incubated in PBS for an equivalent time. The effect of prolonged exposure times was investigated for up to 3 h in terms of cell viability. After exposure, PBS was removed and the cells were incubated in fresh media until required for assessment of osteoblast function, with media being refreshed every 2-3 days for the duration of the experiment.

Markers of osteoblast function
Cells were seeded at 2×10⁴ cells/cm² in 96-well plates for measurement of alkaline phosphatase (ALP) activity, collagen synthesis and osteocalcin expression. ALP activity was measured at 24 and 72 h post-exposure to 405 nm
HINS-light at irradiances between 0.5 and 15 mW/cm² by the dephosphorylation of p-nitrophenyl phosphate (pNPP; 1 mg/mL). DMEM was removed, wells washed with PBS, and 200 μL of 1 mg/mL pNPP in 0.1 M glycine buffer, pH 10.4, containing 1 mM MgCl₂ and 1 mM ZnCl₂, added to each well. pNPP is dephosphorylated to p-nitrophenol and phosphate in the presence of ALP, and the resultant release of p-nitrophenol was detected at 405 nm immediately and 15 min after addition and calculated using the extinction coefficient of p-nitrophenol (18.75 mM/cm) (Bowers and McComb, 1966).

Collagen synthesis by the osteoblasts was assessed by the method of Walsh et al. (1992). At 24 and 72 h post-exposure to 405 nm HINS-light at irradiances between 0.5 and 15 mW/cm², the cells were fixed by Bouin’s solution, and stained with picrosirius red stain for 1 h. Following a wash with 0.01 M HCl, cells were solubilised in 0.25 M NaOH, and the absorbance quantified at 550 nm using a microplate reader.

Culture and 405 nm HINS-light exposure of bacterial pathogens
Culture collection strains of Staphylococcus aureus NCTC 4135 and Staphylococcus epidermidis NCTC 11964 were obtained from the National Collection of Type Cultures (Collindale, UK). Clinical bacterial isolates used in this study were Staphylococcus aureus, Staphylococcus epidermidis, Corynebacterium striatum, Enterococcus faecalis, Micrococcus sp., Escherichia coli, Klebsiella pneumoniae, Serratia marcescens and Pseudomonas aeruginosa. All clinical isolates were isolated from infected hip and knee arthroplasties, and were obtained from the Southern General Hospital Microbiology Department (Glasgow, UK).

For experimental use, bacterial species were inoculated into 100 mL broth (Oxoid/Thermo Fisher Scientific, Basingstoke, UK) and incubated at 37 °C for 18 h under rotary conditions (120 rpm). All microorganisms were cultured in Nutrient Broth (Oxoid/Thermo Fisher Scientific) with the exception of C. striatum, which was inoculated in Brain Heart Infusion Broth (Oxoid/Thermo Fisher Scientific). After incubation, cultures were centrifuged at 3939 × g for 10 min and the microbial cell pellet was then re-suspended in 100 mL PBS. Bacterial suspensions were diluted to a population density of 10⁶ colony-forming units per millilitre (CFU/mL). For 405 nm light exposure, 100 μL microbial suspensions were seeded onto agar plates, providing a population of approximately 100-300 CFU/agar plate. Nutrient agar was used for all bacterial species except C. striatum, which was seeded onto blood agar (Oxoid/Thermo Fisher Scientific).

For exposure of S. aureus NCTC 4135 and S. epidermidis NCTC 11964, the 405 nm HINS-light source used was the same as that used for exposure of the osteoblast cells. Microbial samples were exposed to 1 h durations of 405 nm light with an irradiance level of 5 mW/cm² (~18 J/cm²). Post-exposure, plates were incubated at 37 °C for 24 h before enumeration. Results represent the mean of a minimum of triplicate replicates, and are reported as the percentage of surviving CFU/plate, as compared to non-exposed control samples. To determine the biocidal activity of 405 nm HINS-light against the range of clinical infected arthroplasty isolates, a 405 nm LED array with 144 LEDs (Enis/Photonstar Technology, Romsey, Hampshire, UK) was used which provided an average irradiance of 71 mW/cm² across the diameter of the agar surface. This higher power 405 nm light source provided higher irradiance, thereby providing a more rapid and convenient exposure system for determination of the susceptibility of the range of arthroplasty isolates to 405 nm light. Isolates seeded on the agar surfaces were exposed to increasing durations of light treatment (between 2.5 min to 1 h), and non-exposed control plates were set-up for all samples. As with the culture collection isolates, results are reported as the percentage of surviving CFU/plate, as compared to non-exposed control samples.

Statistical analysis
Data were compared by ANOVA followed by Dunnett’s post-hoc test, unless otherwise stated, and significance was assigned at p < 0.05.
Results

Effect of 405 nm HINS-light exposure on osteoblast function

The function of osteoblasts following exposure to 405 nm HINS-light was monitored by ALP activity and by the ability to synthesise collagen and osteocalcin.

A 1 h exposure to intensities of 405 nm HINS-light at or below 5 mW/cm$^2$ (18 J/cm$^2$) caused no significant reduction in activity of ALP at 24 h post-exposure. Intensities above 5 mW/cm$^2$ caused a statistically significant decrease in ALP activity. By 72 h post-exposure, osteoblasts treated at 15 mW/cm$^2$ showed minimal signs of recovery. Cells exposed to 5 mW/cm$^2$ HINS-light and below did not show a significant decrease in ALP activity compared with the control at 72 h post-exposure (Fig.1).

Differential interference contrast (DIC) microscopy images of control cells and cells exposed to 1 h of 15 mW/cm$^2$ HINS-light stained with picrosirius red for the presence of collagen are shown in Fig. 2 (A) and (B) respectively. Microscopy was performed at 48 h following exposure. Osteoblasts exposed to 15 mW/cm$^2$ retained the elongated shape of healthy osteoblasts and no obviously damaged cells were present in the sample. Collagen synthesis was not affected by exposure to up to 5 mW/cm$^2$ HINS-light, at either 24 or 72 h post-exposure. A significant decrease in synthesis was shown in osteoblasts exposed to 15 mW/cm$^2$ HINS-light at 24 h post-exposure, and this significant decrease persisted at 72 h post-exposure (Fig. 3) with no sign of recovery.

No decrease was observed in osteocalcin expression by osteoblasts exposed to 5 mW/cm$^2$ or lower HINS-light for 1 h at up to 10 days post-exposure. However, expression was significantly suppressed in osteoblasts exposed to HINS-light intensities of 15 mW/cm$^2$ for 1 h at 3 and 6 days post-exposure (Fig. 4). By 10 days post-exposure, expression of osteocalcin in cells exposed to 1 h of 15 mW/cm$^2$ was not significantly different from the control.

To detect any effects on cell morphology, scanning electron microscopy was performed on cells immediately following a 1 h exposure to 5 and 15 mW/cm$^2$ HINS-light. Cells that had not been exposed to HINS-light had classic osteoblast morphology (Fig. 5A). They appear well attached and stretched out, and high magnification images of individual cells showed no remarkable surface features. Osteoblasts exposed to 1 h at 5 mW/cm$^2$ appeared to be similar to the controls (Fig. 5B), but after exposure to 15 mW/cm$^2$ they had a noticeably different appearance compared to control cells (Fig. 5C). Although the cell density appeared similar, the proportion of cells that were attached and stretched out was less. Higher magnification images of the cell surface showed many small imperfections, like cuts or folds in the membrane, suggesting some sub-lethal effects on the cells (Fig. 5C). A summary of the effects of the maximum dose (15 mW/cm$^2$ for 1 h) of HINS-light on the cells is shown in Table 1.

Having determined that exposure to 5 mW/cm$^2$ for 1 h was a safe dose of 405 nm HINS-light in terms of the osteoblast functions, cells were exposed to this irradiance level of light for up to 3 h to establish the maximum duration this irradiance of light could be used safely. Viability of the cells in culture was measured 48 and 72 h post-exposure by both total protein content and DNA.
staining with Crystal Violet in attached cells. Data in Fig. 6 show that cells tolerated exposure to 5 mW/cm² HINS light for up to 120 min without significant loss of viability, but 3 h exposure resulted in a significant difference in the number of viable attached cells compared with the cells exposed for 60 min.

**Effect of 405 nm HINS-light exposure on bacterial pathogens**
Osteoblast exposure determined that 1 h exposure to 5 mW/cm² light was non-detrimental to the osteoblast cells. Experiments were carried out to assess whether this level of exposure could induce a bactericidal effect in *S. aureus* and *S. epidermidis*. Results, shown in Table 2, demonstrate that exposure to 5 mW/cm² for 1 h successfully reduced bacterial contamination, with a 98% and 83% reduction in population achieved with *S. aureus* and *S. epidermidis*, respectively.

Exposure of a range of clinical isolates from infected arthroplasties demonstrated that 405 nm HINS-light has a non-selective bactericidal effect, with successful inactivation achieved across a wide range of Gram-positive and Gram-negative species (Fig. 7A and B, respectively). Inactivation of Gram-positive species appeared to occur at a slightly faster rate with >90% inactivation occurring between 5-30 min, compared to 10-60 min for the Gram-negative species. When comparing the inactivation data for the clinical *S. aureus* and *S. epidermidis* isolates with those of the culture collection isolates it can be seen that use of the higher irradiance of 71 mW/cm² resulted in much faster inactivation than when using the lower 5 mW/cm² irradiance; 90-100% inactivation in 5-10 min compared...
to 80-100 % after 1 h. These results demonstrate that the higher the irradiance of 405 nm light, the faster the rate of bacterial inactivation that can be achieved.

**Discussion**

The results of this study demonstrate that intensities of HINS-light of 5 mW/cm² and below applied over 1 h, do not have a significant effect on osteoblast function in terms of ALP activity, collagen synthesis and osteocalcin secretion. It is important to state that in all experiments carried out on osteoblasts in this study, culture medium was replaced with phosphate buffered saline (PBS) for the duration of HINS-light exposure due to possible generation of ROS in the culture medium. Cell viability has been shown to be significantly reduced by exposure to visible and near-UV radiation when exposed in culture medium compared to PBS (Stoien and Wang, 1974; Smith, 2009). The main component of culture medium responsible for ROS generation has been shown to be riboflavin, with tryptophan, tyrosine, pyridoxine and folic acid all enhancing the effect (Grzelak et al., 2001).

*In vitro*, ALP activity is well established as a measure of osteoblast ability to synthesise bone (Hoemann et al., 2009), and it is encouraging to find that exposure to 5 mW/cm² for 1 h has no inhibitory effect on the activity either immediately, or after 24 or 72 h post-exposure. As the intensity was increased from 5 to 15 mW/cm² significant decreases relative to control values were observed at both 24 and 72 h post-exposure. The effect of blue light on ALP activity has not previously been investigated in osteoblasts. Low doses of red laser light have been shown to be without significant effect (Khadra et al., 2005) but inhibition at high doses (2 J/cm²) of light at a wavelengths of 670 nm has been reported (Stein et al., 2005).

Collagen synthesis is an essential aspect of bone matrix formation by osteoblasts, and the effects of 405 nm HINS-light exposure on this parameter were found to be similar to the effect on ALP activity. Exposure to intensities of up to 5 mW/cm² for up to 1 h had no significant effect on the ability of osteoblasts to synthesise collagen, while exposure to higher intensities significantly reduces this function. Although collagen synthesis has been shown to be both stimulated (Stein et al., 2005; Saracino et al., 2009) and inhibited (Marques et al., 2004) by laser irradiation, there are no studies in the literature using an equivalent irradiance of light to that used in the present study. Staining of the collagen with picrosirius red and visualising the stained cells by microscopy proved not to be sensitive enough to detect the inhibition of synthesis in the cells, but revealed the morphology of the cells post-exposure to 405 nm HINS-light very clearly. There was no visible evidence of a change in cell morphology, or the presence of apoptotic cells.

Osteocalcin is the most abundant non-collagenous protein produced by osteoblasts, and studies on knock-out mice suggest that it has osteogenic regulatory functions (Ducy et al., 1996). The ELISA kit used in this study has been shown to be an effective reliable method for determining osteogenic potential (Nakamura et al., 2009). As reported previously, osteoblasts did not secrete measurable amounts of osteocalcin without stimulation with the hormone 1,25-dihydroxy vitamin D₃ (Carpenter et al., 1998). Expression of osteocalcin is lower during the log phase of growth of the osteoblasts, and at maximum levels once the cells have reached confluence as reported previously (Owen et al., 1991). Measuring osteocalcin production 3 days after exposure showed that 405 nm
Fig. 5. SEM micrographs showing the effect of a 1 h exposure to 5 and 15 mW/cm² (B and C) HINS-light on osteoblast morphology. Control (A). Scale bars are 5 µm.

Fig. 6. Viability of osteoblasts following exposure to 5 mW/cm² HINS-light for 1, 2 and 3 h. A shows the Crystal Violet staining of cultures incubated in the presence of 5 mW/cm² HINS-light, and control cultures incubated in the absence of HINS-light. B shows the protein content of cultures incubated in the presence of 5 mW/cm² HINS-light, and control cultures incubated in the absence of HINS-light. (*p < 0.05, unpaired student t-test, comparing the controls and HINS light treated samples after the same exposure time, n = 4 independent experiments ± SEM).
HINS-light doses of up to 5 mW/cm² did not significantly affect expression, whereas exposure to 15 mW/cm² caused a significant reduction, from which the cells had recovered 10 days after exposure. There are no data in the literature on the effect of blue light on osteocalcin expression in osteoblasts, but near-UV laser irradiation has been shown to stimulate osteocalcin production in human osteoblasts (Khadra et al., 2005).

SEM analyses showed that exposure to 5 mW/cm² did not cause any visible difference to the cell morphology compared to control cells, and the density of the cells was not significantly reduced. However, after the osteoblasts were exposed to 15 mW/cm² for 1 h there was undoubtedly some disturbance caused to the membrane of the cells. The resolution of the images is not high enough to identify the features, but they may represent the initial stage of bleb formation. The decrease in surface area observed after exposure to 15 mW/cm² HINS-light confirms an effect on the cells, and may represent the shrinking associated with apoptosis. A lesser percentage of cells in this group had the stretched morphology and associated large surface seen in the control cells.

The results demonstrate that 405 nm HINS-light has a dose dependent effect on osteoblast function. They imply that irradiances of up to 5 mW/cm² delivered over a period of 2 h should not cause damaging effects to osteoblasts during procedures such as hip replacement, which result in exposure of bone surfaces to the external environment. The time required for implantation of a primary hip arthroplasty is approximately 1 h surgery, and a revision operation is considerably longer; 2 to 2.5 h depending on the complexity of the case. The data shown here illustrate that exposure to HINS-light, under the conditions used for up to 120 min, does not significantly alter osteoblast viability. However, we recognise that the cells used were derived from rat tissue, and there may be differences in the responses of human cells.

Despite the finding that a 1 h exposure to 15 mW/cm² irradiance HINS-light has detrimental effects on osteoblast function, this may have no significant bearing on bone formation or osseointegration of implants during use of the light in a surgery environment. Light of 405 nm wavelength will not penetrate deeply into bone. Penetration of the visible light spectrum into tissue increases with wavelength, with red light penetrating the skin to 6 mm, and shorter wavelength blue light only penetrating up to 2 mm (Fernandez-Guarino et al., 2007). Macrene (2006) also showed that 50 % of red light photons (wavelength 800 nm) would penetrate 20 mm into soft tissue, compared with 80 μm for photons of 255 nm UV light. Although data on the penetration of blue light are not available, porcine studies have shown that a 4.3 mW/cm² laser of 635 nm light penetrates 1.6 ± 0.4 mm into trabecular bone (Bisland and Burch, 2006). Any damage to osteoblasts in this context would therefore only occur on the bone surface, and would have only limited effects on osseointegration of an implant. Osseointegration is not a surface process and, during total hip replacement, osseointegration of the femoral stem will take place deep within the cavity of the bone, where exposure to 405 nm HINS-light will be minimal. It is therefore unlikely that 405 nm HINS-light at the intensities and duration used in this study would cause any significant delay in osseointegration of implants.

It was important to establish that, whilst being non-detrimental to the osteoblast cells, exposure to 5 mW/cm² 405 nm HINS-light for 1 h was capable of inducing a bactericidal effect on bacterial contamination. S. aureus and S. epidermidis were selected for use due to their significance as causative pathogens of arthroplasty infections (Hamilton and Jamieson, 2008; Wilson et al., 2008), and at this dose bacterial kill of 98.1 % and 83.2 % were obtained, respectively, demonstrating a potent bactericidal effect against the culture collection isolates. The bactericidal efficacy of HINS-light against clinical isolates from infected hip and knee arthroplasty tissue from the Southern General hospital in Glasgow was convincingly shown for a range of Gram-positive and Gram-negative bacteria. A comparison of the inactivation
The experiments described in this study were carried out under closely defined laboratory test conditions and have established critical dose levels for safe exposure of osteoblast tissue to 405 nm light. For practical application, this dose level will be dependent on the irradiance from the light source, the distance from the treated tissue and the exposure time. It is anticipated that for the proposed practical application, 405 nm disinfecting light systems would have brightness characteristics similar to typical operating theatre lighting. Further work, involving close interaction with surgical staff, is required to translate these findings into the optimal design of a light-delivery system, which could potentially have application for directed continuous disinfection of the operating environment during real-time arthroplasty surgery.

Conclusions

405 nm HINS-light exposure for 1 h at 5 mW/cm² does not significantly alter osteoblast morphology, function or viability. It is an effective bactericide for clinically relevant bacteria and was found to kill 98.1 % of *Staphylococcus aureus* and 83.2 % of *Staphylococcus epidermidis* populations at this dose. These findings, along with the limited penetration of the light into tissues, suggest that 405 nm HINS-light at this exposure level could potentially be used for directed environmental disinfection in orthopaedic operating theatres. In fact, osteoblasts exposed to 5 mW/cm² for up to 2 h showed no loss of viability. For localised short duration exposure, such as during high risk surgical procedures, 405 nm HINS-light has potential to be used to reduce the number of airborne and surface bacteria in the area immediately surrounding a surgical site without damaging the exposed tissues, analogous to the results from environmental disinfection procedures already demonstrated in the Burns Unit of Glasgow Royal Infirmary. This visible light-based technology has the potential significantly to reduce contamination, and consequently infection, in arthroplasty, and has applications in many diverse areas of surgery, particularly where medical devices are being introduced into the body.

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**Editor’s note:** All questions and comments by the reviewers were answered by text changes. Hence there is no “Discussion with Reviewers” section.