TIME-FREQUENCY TRANSFORM BASED PANIC DISORDER CLASSIFICATION

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Abstract - Event-related brain potentials (ERP) within the electroencephalogram (EEG) can be used to differentiate between the responses to neutral or panic disorder triggering stimuli when presented to anxiety patients. In this paper, we employ time-frequency (TF) revealing transforms to identify a small number significant parameterising coefficients that permit us perform — as well as quantify — this differentiation.

1. INTRODUCTION

Individuals with panic disorder suffer from an abnormal fear of certain sensations usually connected to anxiety, such as palpitation, breathlessness, or dizziness [1]. The research into this disorder has been driven by behavioural science as well as clinical applications, and led to studies investigating possible explanations as well as diagnosis of its symptoms by means of appropriate stimulation and measurement of the subsequent ERPs [2, 3]. These have identified a low frequent transient waveform with a latency of approximately 300 ms after stimulus onset, therefore referred to as P300, as a distinctive feature.

A method of detecting the P300 in panic disorder and normal response ERPs is presented in [4] by means of analyses of variance (ANOVAs). Since the P300 has a transient behaviour, the application of time frequency (TF) analysis appears well suited, as it takes both spectral and temporal information into account. Therefore, in this paper we investigate various transforms, such as wavelet, wavelet packet, and Gabor transforms — with respect to their suitability of revealing the TF characteristics of the transient P300. We aim to optimise these transforms such that the distinction between panic disorder and normal responses is concentrated in only very few coefficients which can yield a distinction. Further, we comment on the selection of a set of distinctive coefficients.

2. PANIC DISORDER ERP

For the measurement of panic disorder ERPs, an anxiety patient was presented with fear-inducing or neutral words tachistoscopically at the perception threshold of panic disorder. The patient's perception threshold for correctly identifying 50% of the words was determined with neutral words not used in the experiment. Based on the assumption that he will recognise a greater number of anxiety words given at his perception threshold than neutral words, the hypothesis examined is the expectation that his EEG exhibits an enhanced P300 wave for presented anxiety words [4].

The EEG was measured at the vertex electrode (Cz) synchronously to the stimulus, whereby the recordings were started 100 ms before the onset of the visual word stimulus. The data exemplarily analysed in this study contains 24 neutral word presentations and 24 anxiety word presentations to one panic patient. Fig. 1 shows the average over the stimulus-synchronous EEG in reaction to the 24 words presented for each word category. There is a visible difference in the two averages with a stronger P300 and more positive EEG until approximately t = 700 ms in the panic disorder related data.

3. PARAMETERISING TRANSFORMS

To parameterise the ERPs in Fig. 1, TF transforms lend themselves to account for the transient nature of the waveforms. To capture the impulsive rise of the P300, TF transforms with a good time resolution are required. The discrete wavelet transform generally yields a good frequency resolution and poor time resolution at low frequencies, yielding a too coarse time segmentation in the frequency range of interest. Therefore, instead we consider the wavelet packet (WP) transform, whose level of decomposition can be adapted to fit the nature of the data, as well as the Gabor transform, which yields a uniform tiling of the TF plane and hence can provide a desired resolution in a specific TF segment.

Based on an implementation described in [5], the WP uses Mallat's wavelet [6], whereby the decomposition level of the transformation is adapted to minimise the entropy of the average ERP curves in Fig. 1. The Gabor transform is based on an oversampled filter bank with 64 channels constructed according to [7]. The resulting approximate distribution of the coefficient energies in the TF plane is visualised in Fig. 2.

The application of the transform methods leads to a parameterisation of the ERP data whereby the features of the ERP are expressed in as few coefficients as possible. Within these ERPparameterising coefficients, we will now attempt to isolate those that represent a significant difference between the two data sets.

4. DIFFERENCE EVALUATION

Based on the parameterisations mentioned in the previous section, we want to identify coefficients that allow us to differentiate between the presented anxiety related and neutral words. Here, we apply the *t*-test, which gives the probability that two data sets sampled from potentially two different distributions



Fig. 1. Average over 24 EEG segments showing responses to anxiety related and neutral stimuli at the perception threshold.



Fig. 2. Average coefficient energy for (left) neutral words and (right) panic order related words using (top) WP and (bottom) Gabor transforms.

with identical variance possess different mean values, for which a significance is returned. Comparing sets \mathbf{x}_p and \mathbf{x}_n containing the panic disorder and neutral ERP response coefficients for one specific transform coefficient across all 24 measurements, the *t*-value is given by [8]

$$t = \frac{\overline{\mathbf{x}}_p - \overline{\mathbf{x}}_n}{\sqrt{\frac{\sigma_p^2}{N_p} + \frac{\sigma_n^2}{N_n}}} \quad . \tag{1}$$

The values $\overline{\mathbf{x}}_p$ and $\overline{\mathbf{x}}_n$ represent the means, σ_p^2 , σ_n^2 are the variances and $N_p = N_n = 24$ are the number of samples for the two data sets. The *t*-value corresponds to a certain significance level *P*, which can be looked up from tables [8]. A smaller value for *P* indicates that the data sets have a significantly different mean. For example, for P = 0.01 the probability that the differences in the means are due to a sampling error is 1%. For our study, a significance level of P = 0.01 was used to identify distinctive coefficients. The two tested distributions were the distributions for one coefficient over the presented 24 neutral and anxiety words, respectively.

5. RESULTS AND DISCUSSION

As discussed in Secs. 4 and 3, we have different transform methods and a procedure to identify significant coefficients to being able to separate between presented neutral and anxiety words. In the following, we will discuss the used transforms and present the results for separability which we obtained for the data described in Sec. 2.

5.1. Transform Adjustment

The optimal decomposition structure for the WP is found over minimising the entropy as mentioned in Sec. 3. The decomposition depth was limited to have at least 16 coefficients in one decomposition level as further decomposition would lead to a too coarse time segmentation. In terms of the Gabor transform, various filters were tested and it was found that using a prototype filter with length of 448, a frequency segmentation of 64 uniform scales and a time segmentation of 14 for the oversampling shows the best results.

5.2. Identified Coefficients and Difference Comparison

Fig. 3 shows the resulting coefficients when performing the t-test on the parameterised data. We see that two coefficients (black and grey) for both transforms are identified. They cover approximately the area of the P300 slow wave as it is expected in Sec. 2. Fig. 4 shows the difference of the averages of the



Fig. 3. Resulting coefficients for (left) WP and (right) Gabor transforms.



Fig. 4. Difference of neutral and anxiety EEG data compared with its parameterisation by the two identified coefficients for (top) WP and (bottom) Gabor transforms.

neutral and anxiety EEG compared with its parameterisation by the identified coefficients for the two investigated transforms. It can be observed that the two identified WP coefficients parameterise the P300 area very well. However, the Gabor transform shows only a small but still clearly noticeable parameterisation of the difference.

6. CONCLUSIONS

We have presented a WP and Gabor transforms analysis comparison for parameterising ERP with the aim of differentiating between presented neutral and anxiety words to a patient with panic disorder. We have motivated the use of TF methods, and proposed an approach to obtain distinctive transform coefficients. The obtained results appear reasonably robust and encourage panic disorder classification via TF analysis of ERP.

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