

Increased dissolution rates of tranilast solid dispersions extruded with inorganic excipients

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ABSTRACT

The purpose of this study was to evaluate the performance of Neusilin® (NEU) a synthetic magnesium aluminometasilicate as inorganic drug carrier co-processed with the hydrophilic surfactants Labrasol and Labrafil to develop Tranilast (TLT) based solid dispersions using continuous melt extrusion (HME) processing. Twin – screw extrusion was optimized to develop various TLT/excipient/surfactant formulations followed by continuous capsule filling in the absence of any downstream equipment. Physicochemical characterisation showed the existence of TLT in partially crystalline state in the porous network of inorganic NEU for all extruded formulations. Furthermore, in-line NIR studies revealed a possible intermolecular H-bonding formation between the drug and the carrier resulting in the increase of TLT dissolution rates. The capsules containing TLT extruded solid dispersions showed enhanced dissolution rates and compared with the marketed Rizaben® product.

Keywords: extrusion, solid dispersions, inorganic excipients, drug – excipient interactions dissolution.

1. Introduction

The pharmaceutical industry is currently in the process of undergoing a transition from conventional batch manufacturing production to continuous processing. Due to market globalization, big pharmaceutical companies are facing immense challenges to comply with the demands of regulatory agencies, while the reduced lifespan of patents and overall decreased profitability of newly discovered drug substances are forcing them to shorten the drug development times with maximum throughput. Therefore, continuous manufacturing processes (CM) can be proved an efficient and promising alternative for achieving these goals [1]. CM provides better product quality assurance than batch processes, with less labor cost and development time. Furthermore, strong efforts are taken on the implementation of process analytical tools (PAT) for the purposes of in-line process monitoring and quality control [2-4].

To date, hot melt extrusion (HME) has been utilised to a great extent for the development and optimisation of solid dispersions [5-14] in order to enhance the dissolution rate of water insoluble drugs [15-16]. Although HME is a versatile technology and can be used for continuous manufacturing of various pharmaceutical dosage forms, it has yet to be fully exploited for such purposes. Continuous HME offers several advantages such as small footprint, cost efficiency, reduced material waste and coupling with various PAT tools.

The processing of inorganic excipients [17,18] as drug carriers to increase dissolution rates of water insoluble drugs has recently gained interest for the development of solid dispersions. Bahl *et al.*, evaluated the solubility and dissolution profiles of the poorly water-soluble drug indomethacin co-processed with Neusilin, an inorganic carrier, [19] using ball-milling micronization. The author found that the presence of silicic acid and Mg^{2+}/Al^{3+} ions, of NEU in the dissolution media increased the concentration of indomethacin and enhanced its *in vitro* dissolution rates. Maclean *et al.* (2011), described a robust extrusion process involving HME to form a Sulindac-NEU amorphous drug complex to enhance the dissolution rate of sulindac [20].

Recently, Maniruzzaman *et al.*, conducted extrusion studies to assess the performance of synthetic magnesium aluminometasilicate as an inorganic carrier for the development of stable indomethacin (IND) solid dispersions. Several IND/NEU blend ratios (20%, 30% and 40%) were extruded continuously using a twin - screw extruder resulting in enhanced drug dissolution rates while the solid dispersions were stable for over 12 months [21]. The same group reported another study of an extrusion granulation process for the increased dissolution of the water insoluble ibuprofen (IBU). A quality-by-design (QbD) approach was

implemented through a design of experiment to produce IBU loaded granules. The extruded granules showed significant enhancement in the dissolution profiles of ibuprofen, which were attributed to the intermolecular interactions of the drug and inorganic carrier [22].

Neusilin® (NEU) is considered a synthetic magnesium aluminometasilicate [23] that exhibits exceptional physical properties for improved drug delivery (e.g. high specific surface area, high flowability, amorphous). Tranilast (TLT) is classified as a BCS class II drug with solubility in water and acidic medium (pH 1.2) of 14.5 and 0.7 µg/mL, respectively [24,25]. Several studies have been reported on the development of TLT dosage forms including solid dispersions and nanoparticles [26-29]

Up to date most of the research focuses on the HME processing of polymers, lipids or inorganic excipients as single drug carriers. Herein we present a two-fold study where inorganic excipients are co-processed with a variety of surfactants/solubilizers to produce stable solid lipid dispersions with enhanced drug dissolution rates. In addition, HME processing was optimized for continuous manufacturing of TLT capsules by direct feeding of the extruded formulations in a capsule-filling machine.

2. Materials and method

2.1 Materials

Tranilast (TLT) ($\geq 98\%$) was purchased from Tokyo Chemical Industries (Japan) and Neusilin (NEU) ($\geq 99\%$) was kindly donated by Fuji Chemical Industries Co., Ltd. (Japan). Labrasol (LSOL) ($\geq 98\%$) and Labrafil (LFIL) ($\geq 98\%$) were kindly donated by Gattefosse, France. All solvents used were of analytical grade and used as received.

2.2 Solubility study of TLT in surfactants

The phase solubility studies were performed to determine the solubility of TLT in the presence of various surfactants in a buffer solution (pH 6.8). An excess quantity of TLT was placed in 20 ml tube containing 10 ml of buffer medium with 1-5% surfactants (w/w). All test tubes were subjected to sonication for 20 min at room temperature followed by exposure to orbital shaking thermo stable incubator (Boekel Scientific, Germany) for 48 h at $37 \pm 0.5^\circ\text{C}$ with rotating speed of 75 agitations /min. The supernatant solution was then passed through Whatman filter Paper (Grade 1) and analyzed by HPLC to quantify the amount of TLT dissolved. The best two surfactants were chosen to undertake further experiments.

2.3 Continuous hot-melt extrusion processing and manufacturing of capsules

The prepared binary and ternary mixtures with either LSOL or LFIL as surfactants were extruded at temperatures varying from 170–200°C to find the suitable extrusion processing parameters (Table 1). The temperatures, screw speed and the torque forces were recorded for each processed sample. The screw speed used for extrusion was 50-100 rpm with a feed rate of 1 kg/hr. The EuroLab 16 (Thermo Fisher, Germany) is connected to a terminal PC where the processing parameters are controlled through the appropriate software supplied by Thermo Fisher. The extrudates were collected in powder form and no additional downstream processing was required. Upon optimization of the extrusion process, the temperature of the final zones was set at 180 °C.

All extruded granules were fed to a Mini Cap capsule filler (Karnavati Engineering Ltd, India) in line with the extruder in continuous manufacturing platform (Fig. 1). The machine output was set at 1500 capsules (0 size) per hour in automatic mode.

2.4 Scanning electron microscopy (SEM)

A cold-cathode field-emission gun scanning electron microscope (Hitachi SU8030 FEG-SEM, Japan) was utilized to evaluate the extrudates spatial distribution of discrete chemical phases. The samples were placed on double-sided carbon adhesive tabs and coated with carbon (Edwards 306 high vacuum carbon evaporation) before SEM analysis. The surface analysis to characterize the morphology of the pellets was evaluated using SEM at a nominal magnification of $1000\times$ (area = 0.127 mm \times 0.095 mm). The accelerating voltage of the incident electron beam was set at 8 kV. This value was selected in order to minimize beam damage to the sample while maintaining adequate excitation.

2.5 Particle size analysis

The particle size distributions of the granules were determined using a Mastersizer 2000 laser diffraction instrument (Malvern Instruments, UK) with a dry powder sample dispersion accessory (Scirocco 2000) and pressure at 0.5 bar and a vibration feed rate of 50%. Samples were run in triplicates. Mastersizer 2000 software was used for data evaluation.

2.6 Thermal analysis

A Mettler-Toledo 823e (Greifensee, Switzerland) differential scanning calorimeter (DSC) was used to carry out DSC runs of pure actives, physical mixtures and extrudates. 2-5 mg of sample was placed in sealed aluminium pans with pierced lids. The samples were heated at 10°C/min from 0°C to 220°C under dry nitrogen atmosphere and reheated at the same heating rate.

Thermogravimetric analysis (TGA) measurements were conducted synchronously on a Q5000 (Thermal Analysis Company, USA). The vesicle samples were frozen in a liquid nitrogen bath followed by a vacuum freeze-drying step before TGA and DSC measurements. The lyophilized samples were placed into the alumina crucible with nitrogen as the reference. The heating-rate was 10°C/min from 25 to 250°C.

2.7 X-ray powder diffraction (XRPD)

XRPD was used to determine the solid state of pure active substances, physical mixtures and extruded materials using a Bruker D8 Advance (Germany) in theta-theta mode. For purposes of this study a Cu anode at 40kV and 40Ma, parallel beam Goebel mirror, 0.2 mm exit slit, LynxEye Position Sensitive Detector with 3° opening (LynxIris at 6.5 mm) and sample rotation at 15 rpm were used. Each sample was scanned from 2 to 40° 2 θ with a step size of 0.02° 2 θ and a counting time of 0.1 seconds per step; 176 channels active on the PSD making a total counting time of 35.2 seconds per step.

2.8 In-line Near Infra-Red (NIR) monitoring

Near infrared spectrometry was performed during extrusion using an Antaris II NIR spectrometer (Thermo Scientific, UK) equipped with a halogen NIR source and InGaAs detector. The instrument utilised a fibre optic probe which was connected to the NIR spectrometer and used for in-line monitoring. NIR spectra were collected in real-time during the entire extrusion process via a fibre optic diffuse reflectance probe. All NIR in-line spectra were continuously collected using the RESULT Integration software (Version 3.0 Thermo Scientific, UK). Each spectrum was acquired by averaging 32 scans with a resolution of 16 cm⁻¹ over the 4,000–10,000 cm⁻¹ wavenumber range. The acquisition of a full spectrum took approximately 16 s. The spectral pre-processing was performed using the TQ Analyst software (Version 8.6.12 Thermo Scientific, UK).

2.9 *In vitro* dissolution study

In vitro dissolution studies [30] were conducted in 900 ml of 0.2 M dihydrogen-sodium-orthophosphate (pH adjusted with NaOH to 6.8) for 2 h using a Varian 705 DS dissolution paddle apparatus (Varian Inc. North Carolina, US) at 100 rpm. All formulations were directly dropped in the vessels without filling them in a capsule (n=3). Dissolution bath and vessels were equilibrated to $37 \pm 0.5^{\circ}\text{C}$. Samples were withdrawn for HPLC assay at predetermined time intervals.

2.9 HPLC analysis

The release of TLT was determined by using HPLC, Agilent Technologies system 1200 series. A HYCHROME S50DS2-4889 (5 μm x 150 mm x 4mm) column was used for the HPLC analysis. The wavelength was set at 340 nm. The mobile phase consisted of methanol/water/triethyl amine (75/25/0.2 v/v) and the flow rate was maintained at 1.0 ml/min and the retention time was 2-3 min. Calibration curve was prepared with concentrations varying from 10 μg /ml to 50 μg /ml and 20 μl injection volumes.

3. Results and discussion

3.1 HME processing and capsule manufacturing

In order to optimize the extrusion processing parameters, various TLT based formulations of different ratios and compositions were processed under different extrusion temperatures varying from 170-200 $^{\circ}\text{C}$. The solid-state analysis (see below) revealed that temperatures above 180 $^{\circ}\text{C}$ are the most appropriate for the processing of TLT batches and the drug remained stable within the temperature range (melting point of TLT is above 200 $^{\circ}\text{C}$). Utilizing inorganic silicates as drug carriers during the HME process optimization resulted in the production of free flowing granules. NEU is considered an excellent excipient for extrusion purposes due to its high flowability (Carr's index 13), high specific surface area and the drug absorbance within a silicate porous network [23].

The TLT solubility studies conducted using a range of hydrophilic surfactants (suppl. material) revealed that both Labrafil and Labrasol have the highest solubilisation capacity for TLT in buffer solution (pH 6.8). Therefore, these two grades were used as hydrophilic surfactants and co-processed with NEU at high drug loadings (40-60% w/w ratios) as shown in Table 1. The extrusion of NEU in presence of liquid surfactants (10-15% w/w ratios)

facilitated a complete dry blending resulting in the production of TLT loaded free flowing powders.

The excellent flowability of the extruded powders was also achieved even at 60% drug loadings despite the poor flow properties of TLT and the surfactants used in the formulations. The estimated Carr's index values of TLT/NEU and TLT/NEU/surfactants extruded powders varied from 10-11, which are in the same range of the bulk inorganic NEU. The use of inorganic NEU and the process optimization in the absence of the extrusion die eliminated further downstream processing and provided high throughput of extruded formulations. Furthermore, HME was coupled successfully with a MiniCap auto capsule filler to manufacture capsules without the addition of other excipients. The process was allowed to operate continuously for 3hr and produced 1500 capsules ('0' size) per hour.

3.2 SEM and particle size analysis

SEM analysis was used to investigate the surface morphology of the bulk substances and the extruded formulations. As shown in Fig. 2a for all of the TLT/NEU formulations with or without surfactants no drug crystals can be identified on the NEU surface indicating excellent extrusion processing. Further observation shows that TLT/NEU extrudates formed agglomerates comprising of microstructured particles. The formation of agglomerates where the drug substance is adsorbed while the obtained particle size is similar to that of bulk NEU can be of great interest for the development of oral dosage forms (e.g. capsules) in a continuous manufacturing process without the requirement of further down-streaming processing. As shown in Fig. 2b the determined particle size distribution of all extruded batches and bulk NEU varied from 40 – 300 μ m ($d(0.9) = 300\mu$ m). Due to the drug/surfactant adsorption in the porous inorganic network further micronization was not required.

3.3 Thermal analysis

The bulk materials, physical mixtures and extruded formulations were further investigated by DSC analysis. As shown in Fig. 3a, pure TLT presented a sharp endotherm corresponding to its melting peak at 213°C ($\Delta H = 155.27$ J/g). Synthetic NEU didn't present any reversible thermal transition below 250°C in modulated DSC (MTDSC) (only a non-reversible thermal transition was seen at 165°C), which could be due to the loss of the two water molecules present in the NEU structure (Supp. Fig. 1).

TLT/NEU (60/40 w/w) physical mixture (F3) showed a sharp endothermic thermal transition due to the melting of the drug at 213°C ($\Delta H = 174.51$ J/g) (Fig. 3a). In contrast in

the extruded formulation a slight shift of the TLT melting endotherm at 211.89°C ($\Delta H = 160.01$ J/g) was observed. As shown in similar studies [31] of porous carriers the endothermic shift simply indicates the co-existence of amorphous and crystalline TLT in the porous network. A similar phenomenon was observed in TLT/NEU/LSOL extruded formulation (F5) with a significant shift of the melting endotherm towards lower temperatures at 202.37°C. In the physical blends of F5, TLT showed a melting peak at 212.19°C, which was shifted at 201.33°C after the extrusion processing. In both cases the shift in the melting peak of TLT can be attributed to the presence of surfactant in the system. The liquid LSOL has partially solubilized TLT facilitating further adsorption in the inorganic carrier. It can also be seen that the melting peaks differ in shape where broader peaks suggest more drug melted within the pores. This indicates that the presence of hydrophilic surfactant such as LSOL may have played a key role in the solubilization of TLT during the extrusion process, which in turn is expected to show an impact in the *in vitro* dissolution rates.

Thermo-gravimetric (TGA) analysis was performed to determine any potential material weight loss as a function of the increasing temperatures. As can be seen in Fig. 3b bulk TLT has not showed any weight loss up to 205°C while bulk NEU showed a net weight loss of about 12.0% at 200°C corresponding to the loss of two molecules. A similar thermal transition was observed in the MTDSC analysis as mentioned above. The bulk LSOL showed weight loss of 5.24% which is expected to not to provide any significant impact in the extruded formulations considering only 10% w/w ratio in the final formulation prior to the extrusion processing. Both the TLT/NEU and TLT/NEU/LSOL extruded formulations exhibited lower weight losses of 5.40% and 3.70% respectively. These weight losses are quite lower compared to bulk NEU suggesting that H₂O molecules were not completely removed when NEU was co-processed with TLT or TLT/LSO.

3.4 X-ray powder diffraction (XRPD) studies

X-ray powder diffraction analysis of bulk substances and extruded granules, was performed in order to examine the physical state of the drug substance. As can be seen in Fig. 4 and Supp. Fig. 2 the diffractogram of bulk TLT showed distinct intensity peaks due to its crystalline structure at 11.06°, 12.17°, 13.78°, 16.67°, 18.64°, 22.41°, 24.63°, 28.46°, 31.07° 2 θ degrees while NEU appeared completely amorphous with no crystalline intensity peaks. The physical blends of all TLT formulations showed identical peaks without any reduction of

the peak intensities due to the presence of crystalline TLT. Similarly, all extruded granules showed identical peaks at relatively low intensities suggesting a lower degree of crystalline TLT is present, alongside an increase of amorphous content during the extrusion processing, even at high 60% drug loading.

3.5 In- line NIR spectroscopy monitoring

Off-line NIR spectra of bulk TLT, excipients and physical blends were recorded in order to identify the characteristic bands of the bulk substances. An in-line NIR reflectance probe was coupled with HME processing to continuously monitor [32,33] all TLT based formulations. Furthermore, in-line NIR spectra of the TLT/NEU 60/40 (w/w) formulation was recorded during the extrusion at the third mixing zone. The second derivative spectra in Fig. 5a-d show a significant peak shift between the NIR spectra of bulk TLT and that in the extruded granules. The NIR signal of NEU was flat in the same region suggesting no effect on the drug absorption. In Fig. 5a it can be seen that the second derivative NIR spectra showed a significant peak shift, particularly in the range of $8800\text{--}8900\text{ cm}^{-1}$, indicating potential intermolecular interactions between the drug and the complex silicate. Interestingly, the dimer peaks of the bulk TLT at $8800\text{--}8900\text{ cm}^{-1}$ disappeared in the extruded granules and showed a broad peak, which could be due to the TLT - NEU interactions but could also be attributed to the increase the amorphicity of the extruded materials.

Furthermore, Fig. 5b shows that a peak at 7095 cm^{-1} attributed to the --OH stretching first overtone of the drug TLT has been shifted to a new position at 7109 cm^{-1} in the TLT/NEU extrudates. The peak shifting at this position is related to the H-bonding between the --COOH of TLT and the --O group of NEU [34]. There are also two more peaks at 7385 cm^{-1} and 7212 cm^{-1} , which were shifted from 7402 cm^{-1} and 7234 cm^{-1} respectively. These two peaks are attributed to the --CH stretching, and the reason of the peak shifting occurs is could be due to the formation of weak H-bond ($\text{C-H}\cdots\text{O}$) between the drug and the excipient [35]. Furthermore, another peak at 5206 cm^{-1} which is attributed to the C=O second overtone has also been shifted to 5230 cm^{-1} (Fig. 5c). This peak shifting is due to the formation of H-bond between the --C=O of the drug and the excipient. The amide group (--CONH-R) of the drug was visible via an intense peak at 4668 cm^{-1} , which has been slightly shifted and appears broader after the extrusion processing (Fig. 5d). This can be attributed to the increase in the

amorphicity of the drug in the extruded formulations as confirmed by the XRD and DSC studies.

3.6 *In vitro* dissolution studies

In vitro dissolution studies of TLT formulations were compared with the bulk TLT and the commercial formulation (Rizaben®). The studies showed a significant improvement of the drug dissolution rates in phosphate buffer (pH 6.8). As shown in Fig. 6a, for the first 60min TLT/NEU extruded (60% TLT loading w/w) formulation and Rizaben® presented similar dissolution rates ($p>0.05$), varying from 70–80%. However, after 120min the extruded formulation presented 100% TLT dissolution rates while Rizaben® reached a maximum of 81-84%. The increase of TLT loading in the extruded formulations resulted in faster dissolution rates for the first 60 min, as shown in Fig. 6a. It can also be seen that the dissolution rate of bulk TLT was approximately 40% after 120 min. No increase in the dissolution rates was observed for the physical mixtures (data not shown). An important observation is that TLT maintained a supersaturation state for 2h which allowed dissolution up to 100%. In contrast Rizaben® capsules containing mainly HPMC reached an 84% drug dissolution after 2h. As primarily the improved dissolution rates are due to the presence of the selected excipients, the low Rizaben® dissolution is a result of the slow HPMC dissolution kinetics compared to NEU and NEU/solubilizer formulations [36,37].

As shown in Fig. 6b for the co-processed NEU/LSOL extrudates the TLT dissolution rates were again similar to Rizaben® at 76% after 30 min but significantly higher after 60 min. The TLT/NEU/LFIL extrudate showed slower dissolution rates with around 61% for the first 60 min compared to TLT/NEULSOL and Rizaben® respectively and 95% at 120 min. Interestingly, both formulations presented lower dissolution rates for the first 60 min in comparison to Rizaben®. The effect of the LSOL/LFIL solubilizers on the dissolution enhancement were evident after the first 30 – 60 min. The dissolution rates of the physical mixtures (Fig. 6 suppl. material) showed a small increase due to the presence of surfactants and rates varied from 48 – 52% after 2hr which, however was not a significant one. These results suggest a surfactant synergistic effect only when co-processed with inorganic NEU.

The observed increase in the dissolution studies of TLT extruded formulations could be attributed to the effect of a) the sinalol groups in NEU, b) the presence of amorphous TLT due to the adsorption in the porous network and c) H-bonding interaction of TLT-NEU. As

previously reported, NEU generates various silanol groups (e.g. free, germinal or associated) when in contact with water render it a potential proton donor as well as a proton acceptor [22]. The existence of free silicic acid and ions (Mg^{2+} and Al^{3+}) in the dissolution media may have played a vital role to cause the increase in the dissolution of TLT. The partially amorphous TLT adsorbed in the extruded formulations facilitates faster dissolution rates compared to the fully crystalline substance in the physical mixtures.

Furthermore, the increased TLT dissolution rates alongside the increased drug loadings in the extruded formulations resulted in stronger drug – excipient interactions. Similar results were observed from Bahl et al. for indomethacin solid dispersions. In the present study, the increased dissolution rates in the presence of LSOL or LFIL within the extruded formulations is due to the solubilising capacity of the two surfactants. However, as shown in Fig. 6b the presence of LSOL in the extrudates resulted in better dissolution rates compared to LFIL due to its better solubilizing effect on TLT as confirmed by the saturation solubility data (Supp. Fig. 3).

As shown in Fig. 4 the granulated formulations presented amorphous TLT to some extent (5-10%) which is expected to have an effect on dissolution rates. Indeed, stability studies under accelerated condition (40°C/40% RH, data not shown) for six months presented a degree of TLT re-crystallization and changes on the dissolution rates. However, statistical analysis didn't reveal any significant changes on the dissolution rates ($p>0.05$) of the stability batches. This was attributed to the protective effect of NEU which promotes long term stability of the extruded granules.

4. Conclusions

In the current study inorganic aluminosilicates were processed with or without surfactants and exploited as a suitable drug carrier for continuous extrusion processing to produce capsules with enhanced dissolution rates of the poorly water-soluble drug TLT. The process comprised of only 3 operational units for continuous extrusion processing followed by capsule filling in the absence of any downstream equipment. The process optimization resulted in 60% TLT loadings with excellent powder flowability of the extruded formulations. Physicochemical characterization showed drug adsorption in the porous inorganic network, while the presence of surfactants increase TLP dissolution rates. *In vitro* dissolution studies revealed a significant increase of the dissolution rates of extruded TLT

formulations compared to that of marketed Rizaben® capsules. Inorganic excipients were used as a paradigm for drug extrusion though continuous capsule filling.

Conflict of interest

The authors report no declaration of interests.

Acknowledgments

This work was financially supported by the Fuji Chemical Industry Co., Ltd., Japan.

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Table 1: Formulation composition of TLT based formulations

Formulation	TLT (w/w)	NEU (w/w)	LSOL (w/w)	LFIL (w/w)
1	40	60		
2	40	30		
3	60	40		
4	60	25	15	
5	60	25		15
6	60	30	10	
7	60	30		10
50/170/180/180/180/180/180/180°C (Feeder to die) Screw speed: 100 rpm, Feed rate: 1 kg/h				

Figures caption list

- Fig. 1** Schematic diagram of manufacturing TLT based capsule in a continuous process.
- Fig. 2a** SEM images of (a-b) TLT/NEU 60/40 and (c-d) TLT/NEU/LSOL 60/30/10 extruded formulations.
- Fig. 2b** Particle size distribution of TLT extruded formulations comparing to the bulk NEU.
- Fig. 3a** DSC thermal transitions of bulk TLT, TLT/NEU 60/40, TLT/NEU/LSOL 60/30/10 and TLT/NEU/LFIL 60/30/10 formulations.
- Fig. 3b** TGA thermograms of bulk TLT, NEU, TLT/NEU and TLT/NEU/LSOL extruded formulations.
- Fig. 4** XRD diffractograms of bulk TLT, NEU and TLT based physical mixtures (PM) and extruded formulations (EXT).
- Fig. 5** (a-d) 2nd derivative NIR spectra of TLT, NEU and TLT/NEU formulations.
- Fig. 6a** *In vitro* TLT dissolution profiles of Rizaben and extruded formulation (n = 3, pH 6.8).
- Fig. 6b** *In vitro* TLT dissolution profiles of Rizaben and co-processed extruded formulations with NEU/LSOL (LFIL) (n=3, pH 6.8).













